



Article Swimming Characteristics of Bioinspired Helical Microswimmers Based on Soft Lotus-Root Fibers

Jia Liu ^{1,2,3}^(b), Tiantian Xu ^{1,2,*}^(b), Yanming Guan ^{1,2,3}, Xiaohui Yan ⁴^(b), Chengwei Ye ⁵ and Xinyu Wu ^{1,2,4}

- ¹ Guangdong Provincial Key Laboratory of Robotics and Intelligent System, Shenzhen Institutes of Advanced Technology, Chinese Academy of Sciences, Shenzhen 518055, China; jia.liu1@siat.ac.cn (J.L.); ym.guan@siat.ac.cn (Y.G.); xy.wu@siat.ac.cn (X.W.)
- ² CAS Key Laboratory of Human-Machine Intelligence-Synergy Systems, Shenzhen Institutes of Advanced Technology, Shenzhen 518055, China
- ³ University of Chinese Academy of Sciences, Beijing 100049, China
- ⁴ Department of Mechanical and Automation Engineering, The Chinese University of Hong Kong, Hong Kong, China; yanxh86@link.cuhk.edu.hk
- ⁵ School of Science and Engineering, The Chinese University of Hong Kong, Shenzhen 518172, China; 116010256@link.cuhk.edu.cn
- * Correspondence: tt.xu@siat.ac.cn; Tel.: +86-0755-8639-2164

Received: 27 October 2017 ; Accepted: 28 November 2017 ; Published: 30 November 2017

Abstract: Various kinds of helical swimmers inspired by E. coli bacteria have been developed continually in many types of researches, but most of them are proposed by the rigid bodies. For the targeted drug delivery, the rigid body may hurt soft tissues of the working region with organs. Due to this problem, the biomedical applications of helical swimmers may be restricted. However, the helical microswimmers with the soft and deformable body are appropriate and highly adaptive in a confined environment. Thus, this paper presents a lotus-root-based helical microswimmer, which is fabricated by the fibers of lotus-root coated with magnetic nanoparticles to active under the magnetic fields. The helical microstructures are derived from the intrinsic biological structures of the fibers of the lotus-root. This paper aims to study the swimming characteristic of lotus-root-based microswimmers with deformable helical bodies. In the initial step under the uniform magnetic actuation, the helical microswimmers are bent lightly due to the heterogeneous distribution of the internal stress, and then they undergo a swimming motion which is a spindle-like rotation locomotion. Our experiments report that the microswimmers with soft bodies can locomote faster than those with rigid bodies. Moreover, we also find that the curvature of the shape decreases as a function of actuating field frequency which is related to the deformability of lotus-root fibers.

Keywords: helical microswimmer; soft fiber; spindle-like rotate; magnetic actuation

1. Introduction

Artificial micro-/nanorobots have attracted lots of researchers to carry on extensive study due to their considerable promise for diverse biomedical tasks such as targeted therapy [1–9], tissue removal [10,11] and micro-manipulation [12–15]. Purcell found the advantages of the nonreciprocal motion and demonstrated two efficient swimming modes at low Reynolds number [16,17]: the flexible oar and the corkscrew. Although Qiu et al. [18] presented a microswimmer that moves with reciprocal periodic body-shape changes in non-Newtonian fluids, its propulsion performance depended on the fluid viscosity upon varying the shear rate. Recently, more attention has been focus on helical magnetic microswimmers which can convert the rotation energy along their helical axis into the translation energy actuated by the uniform magnetic field [2]. Inspired by

mastigoneme structures in nature, the research group from Swiss Federal Institute of Technology Zurich (ETH Zurich) fabricated an artificial helical microswimmers with multiple flagella and mastigonemes, modeled its propulsion model and studied the relation between the length and the velocity [19]. Tabak et al. [20] presented the 6-DOF kinematic models for two-link helical micro/nanoswimmers with the aid of computational fluid dynamics (CFD) analysis. Erman et al. [21] presented three-dimensional trajectory following by means of resistive force theory (RFT) for a rigid helical microswimmer. Nourmohammadi et al. [22] proposed a 3-DOF swimming microrobot with three helical flagella and its dynamical model. Mahoney et al. [23] developed a full 6-DOF model for helical microswimmer and directly controlled its spatial velocity instead of its pitch and rotation speed. Xu et al. [24] analyzed the propulsion characteristic of scaled-up helical microswimmers with different magnetic head or magnetic tail and determined the propulsion matrice. Then Xu et al. [25] accomplished the planar path following based on a 3-D steering scaled-up helical microswimmers. Zhang et al. [26] reported artificial bacterial flagella (ABF) that can swim in a controllable fashion using weak magnetic fields and also analyzed the manipulated performance manipulated by the thrust force. Tottori et al. [27] presented the assembled structure exhibiting the different swimming properties, its dynamic behavior may guide to design active suspensions for drug delivery and imaging. Schamel et al. [28] presented helical nano-propellers showing significant advantages in viscoelastic hyaluronan gels, such as faster or notable propulsion. Walker et al. [29] experimentally analyzed the optimal helix length by trading off between the maximal net chirality and the minimal vicious friction. Similarly, Xu et al. [30] carried on the extended experiment to analysis the four factors (pitch, turn, width, thickness). In all, these researches focused on the swimming characteristics for the rigid body of the helical microswimmer.

Qiu et al. [31] used 3D laser direct writing tool and e-beam deposition methods to manufacture microswimmers with 5 μ m-diameter and 16 μ m-length. Ghosh et al. [32] employed the shadow-growth method to fabricate the glass (SiO₂) nanostructured propellers. Qiu et al. [33] fabricated the helical bodies of ABFs from a available biocompatible photoresist OrmoComp (micro resist technology GmbH, Berlin, Germany), and coated them with Fe. Xu et al. [34] present a swimmer with belt-like soft tail made of polydimethylsiloxane (PDMS). Stanton et al. [35] employed the electrochemical method to fabricate the Ppy microtubes. Li et al. [36] initially used anodic aluminum oxide (AAO) membrane templates with pore diameter of 200 nm for preparing the helical nanoswimmers. In addition, Li et al. [37] employed the template-assisted method to fabricate the bisegment magneto-acoustic hybrid nanomotors. It is a challenge to product the three-dimensional helical micro/nanostructures in a large scale which involves either custom or novel fabrication process, including the optical lithography, two-photon stereo-lithography, self-folding thin-films, micro/nanomachining, micro/nanoimprinting, and micro/nanomolding technique [38]. These fabrication processes can produce a variety of the advanced applications, but they only take place in the laboratory with the specific instrument. Moreover, material used in the fabrication should be biocompatible with respect to in vivo biomedical applications.

In the nature, there are a diversity of microstructures such as plant fibers. Gao et al. [39] proposed plant-based helical microstructures derived from Xylem vessels covered with a thin Ti and Ni layer directly on the spiral vessels, and adopted the propulsion mechanism with respect to the rigidly helical structure, but not described the swimming characteristic in detail. Yan et al. [40] chose the cyanobacterium Spirulina as a based structure to demonstrate the bio-templated synthesis with three steps: precursor deposition, annealing treatment and reduction processing. Employing the physically synthetic methods, we can transform the structures of the plant fiber into the functional microstructures which utilizes their intrinsic natural morphology. Hence, we demonstrate the lotus-root-based magnetically propelled helical microswimmers. The novel helical microswimmers are fabricated by simply coating the lotus-root-based fibers with a thin magnetic layer. Moreover, the lotus-root-based magnetically propelled helical microswimmers can be coated with superparamagnetic nano-particles with manipulated magnetic anisotropy.

The main contributions of this papers are the following: (1) demonstrate the soft and deformable helical microswimmers based on the fibre of the lotus-root; (2) find the spindle-like rotation locomotion; (3) investigate the spindle-like rotation locomotion characteristic.

2. Swimming Characteristic of the Helical Microswimmers

2.1. Theoretical Analysis of Rigid Helical Microswimmers

Purcell suggested that every motion is linear at low Reynolds number, so the propulsion matrix is mapped by the force and torque with the constant coefficient [16]. At low Reynolds number regime, a simplified Stokes equation governs hydrodynamics. An external force applied on the helix that translates along its axis can make it necessarily rotate. An external torque applied on the helix that rotates along its axis also can make it necessarily translate.

Generally, the resistive-force theory (RFT) can calculate the thrust force and torque by the helical motion. The underlying assumption of the intuitive approach is that the hydrodynamic force is proportional to the local body velocity with the constant resistance coefficients (RC) which are derived from the slender body theory. The theory approximates a slender filament by a line distribution of singularity solutions [9].

A helical microswimmer in the fluid at low Reynolds number which is $\text{Re} = \rho u l / \mu$, and the fluid mechanics can be presented by the Stokes equations

$$\begin{cases} \nabla p = \mu \nabla^2 u \\ \nabla u = 0 \end{cases}$$
(1)

where ρ and μ are the density and dynamic viscosity of the fluid, respectively. u and l are the velocity of the objective and characteristic length, respectively. p is the pressure. There is no time-dependent terms in this equation, hinting that the resultant propulsion force only depends on the propeller relative position. Therefore, the microswimmers have to employ non-reciprocal mode in order to locomote forward.

The external force and torque acting on the microswimmer can be modeled by the magnetic force, f_m and τ_m , respectively. The resistive friction force and torque can be presented by f_c and τ_c , respectively. The viscous drag force and torque can be expressed by f_d and τ_d , respectively. With the above analysis, the dynamic equations are given by

$$\begin{cases} \tau_d + \tau_c + \tau_m = 0\\ f_d + f_c + f_m = 0 \end{cases}$$
(2)

When a magnetic field with frequency f_{act} is applied on the magnetized lotus-root-based helical microswimmer. Figure 1 shows the schematic of the helical micro-swimmer and the vicious force f_d and vicious torque τ_d acting on the body due to helical propulsion.

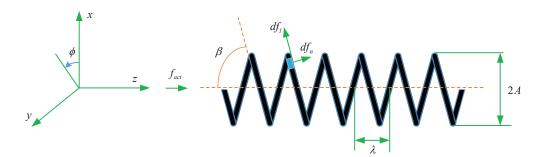


Figure 1. Schematic of the helical microswimmer.

For an element ds on the helix, the propulsive force in *z*-axis direction, in terms of its normal component df_n and longitudinal component df_l , is

$$df_d = df_n \sin\beta - df_l \cos\beta \tag{3}$$

The force df_{ϕ} in ϕ direction is equal to

$$df_{\phi} = -df_n \cos\beta - df_l \sin\beta \tag{4}$$

which results in the vicious torque $d\tau_d$ along *z*-axis

$$d\tau_d = Adf_\phi = -Adf_n \cos\beta - Adf_l \sin\beta \tag{5}$$

where A is the amplitude of the helix and β is the constant pitch angle between the helix and the *z*-axis.

$$\tan\beta = \frac{2\pi}{\lambda}A\tag{6}$$

where λ is the wavelength of the helix.

The velocity vector of the element ds is constructed through the two components of v_n and v_l which arise from the forward movement v and angular movement Af_{act}

$$\begin{cases} v_n = v \sin \beta - A f_{act} \cos \beta \\ v_l = -v \cos \beta - A f_{act} \sin \beta \end{cases}$$
(7)

Hancock et al. [41] proposed theoretical analysis to calculate the normal coefficient C_n and tangential coefficient C_l of viscous resistance on the thin cylindrical filament swimming in a viscous fluid.

$$\begin{cases} df_n = -C_n v_n ds \\ df_l = -C_l v_l ds \end{cases}$$
(8)

The length of segment ds can be rewritten as $ds = dz/\cos\beta$. C_n and C_l are the corresponding coefficients of resistance driven empirically by Johnson and Brokaw [42]

$$\begin{cases}
C_n = \frac{4\pi\mu}{\ln\left(2\lambda/d\right) + 0.5} \\
C_l = \frac{2\pi\mu}{\ln\left(2\lambda/d\right) - 0.5}
\end{cases}$$
(9)

Therefore, substituting (7) into (8), which yields,

$$\begin{cases} df_n = C_n \left(-v \sin\beta + A f_{act} \cos\beta \right) \sec\beta dz \\ df_l = C_l \left(v \cos\beta + A f_{act} \sin\beta \right) \sec\beta dz \end{cases}$$
(10)

The total propulsive force f_d^i and torque τ_d^i on one pitch of the helix can be expressed by integrating the force and torque on the segment *ds* along *z*-axis.

$$\begin{cases} f_d^i = \int_{z=0}^{z=\lambda} df_d \\ \tau_d^i = \int_{z=0}^{z=\lambda} d\tau_d \end{cases}$$
(11)

where *i* is the *i*th pitch.

2.2. Analysis on Spindle-Like Rotation Locomotion Steps

Due to advantage of their intrinsic natural morphology, some synthetic technology can be employed to transform highly structured plant fiber into functional materials. We first utilize the lotus-root fiber to fabricate the propelled helical microswimmers. To obtain stretched spiral fibres, lotus-roots were gently cut, and the two segments were pulled apart to a fixed distance, and then the helixes can be got. The new helical microswimmers are fabricated by the simple coating of lotus-root-based fibers with a thin magnetic layer. Specifically, the lotus-root-based magnetically propelled helical microswimmers can be coated with superparamagnetic nano-particles with manipulated magnetic anisotropy. We adjust the magnetic axis to be approximately perpendicular to the axis of the helical microswimmers are bent lightly initially for different length. Its shaping principle is similar to the strain engineering which is a widely used technique [43]. During the named spindle-like rotation locomotion shown in Figure 2a–d, the microswimmers can locomote with a little sliding actuated by uniform magnetic fields.

The open-loop control of the propulsion of lotus-root microswimmer is achieved by employing a uniform rotating magnetic field. Figure 2a,b shows the two-point-support rotation locomotion step. Within one step period, the two ends of the helical microswimmers touch the bottom of the container and support the whole body to spin 180°. This step is followed by another, as is shown in Figure 2c,d. The apex of the deformable helical body touches the bottom of the container and supports the whole body to spin another 180°. Repeating the process can create the spindle-like rotation locomotion which is different from the rigid rotation locomotion. This spindle-like rotation can both push the helical body to locomote forward perpendicular to p_{axis} and push the helical body side-slide a little bit along p_{axis} . Figure 2 illustrates that v_{side} is parallel to p_{axis} , $v_{forward}$ is perpendicular to p_{axis} .

In another experiment, Figure 3 show the spindle-like rotation locomotion with an inclination angle ϑ but one-terminal of the lotus-root microswimmer touches the bottom of the container. The left one in Figure 3a shows the one-point-support step. Within the step, the one end of the helical microswimmers touches the bottom of the container and supports the whole body to spin 180°. Then for another step, the right one in Figure 3a shows that the one-terminal of the deformable helical body aparts from the bottom of the container and the whole body suspends in liquid spinning another 180°. Repeating the process can create spindle-like rotation locomotion with an inclination angle which can make the helical body to locomote forward perpendicular to p_{axis} .

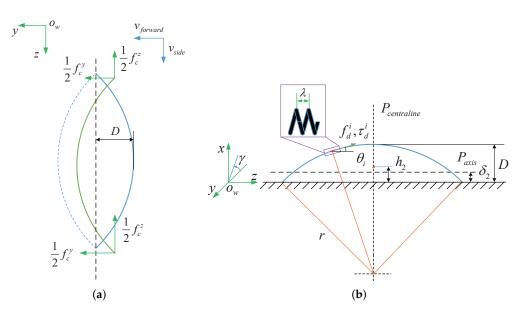


Figure 2. Cont.

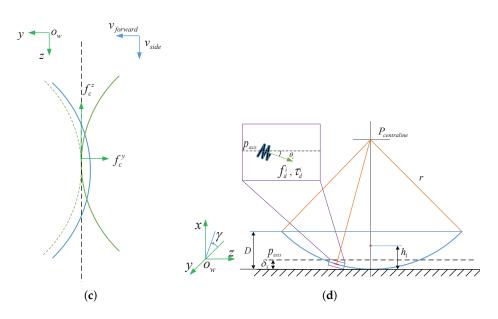


Figure 2. Spindle-like rotation locomotion: Schematic of the two-point-support step (**a**) Spinning 180° along *z*-axis; (**b**) Schematic of the total propulsive force f_d^i and torque τ_d^i on one pitch of the helix, h_2 is the center height from the center position to the bottom; Schematic of the one-point-support step (**c**) Spinning 180° along *z*-axis; (**d**) Schematic of the component propulsive force f_d^i and torque τ_d^i on one pitch of the helix, h_1 is the center height from the center position to the bottom.

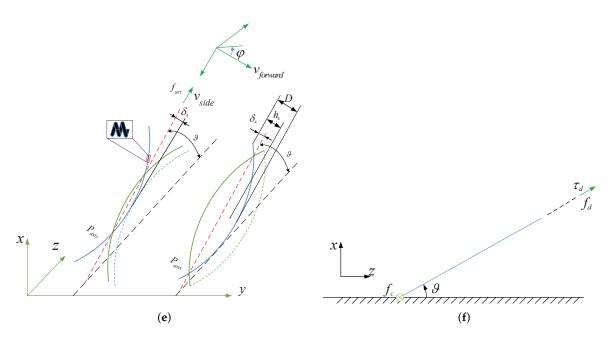


Figure 3. Schematic of spindle-like rotation locomotion with an inclination angle ϑ (**a**) two steps for spindle-like rotation locomotion cycle from top view: zero-point-support step (the left one) and one-point-support step (the right one); (**b**) Schematic of propulsive force f_d , the propulsive torque τ_d , and the friction force f_c from side view.

2.3. Theoretical Analysis of Soft Helical Microswimmers

In order to simplify the dynamic model, we make the assumption that its structure is symmetric about $p_{centraline}$, the following expression along $p_{centraline}$ perpendicular to the instantaneous axis p_{axis} in Figure 2b can be given,

$$\sum_{i=1}^{n} f_x^i \sin \theta_i = 0$$

where f_x^i is the component of the f_d^i along *x*-axis in Figure 2b.

Therefore, the following expression along the instantaneous axis p_{axis} in Figure 2b can be given,

$$\begin{cases} \tau_d = \sum_{i=1}^n \tau_d^i \cos \theta_i \\ f_d = \sum_{i=1}^n f_d^i \cos \theta_i \end{cases}$$
(12)

where *n* denotes the number of the pitch in the whole body, f_d^i and τ_d^i can be obtained from (11),

$$f_d^i = -\lambda \left(C_n \sin\beta \tan\beta + C_l \cos\beta \right) v + \lambda A \sin\beta \left(C_n - C_l \right) f_{act}$$
$$\tau_d^i = \lambda A \sin\beta \left(C_n - C_l \right) v - \lambda A^2 \left(C_n \cos\beta - C_l \sin\beta \tan\beta \right) f_{act}$$

The resistive friction force and torque can be used to model the interactive relation between the robot and the environment. For one step in spindle-like rotation locomotion, the ends of the helical microswimmers touches the bottom of the container and supports the whole body to spin 180°. A simple Coulomb friction model is employed in Figure 2a, which yields

$$\begin{cases} f_c^z = \mu_z \left(\rho_{lotus} - \rho_{liquid} \right) V_{lotus} g\\ f_c^y = \mu_y \left(\rho_{lotus} - \rho_{liquid} \right) V_{lotus} g\end{cases}$$

where μ_z and μ_y are the friction constants, $(\rho_{lotus} - \rho_{liquid}) V_{lotus}$ is the total net mass, *g* is the gravitational constant.

The resultant resistive torque τ_{c2} in Figure 2a,b can be expressed as,

$$\tau_{c2} = 2 \int_0^{\frac{\pi}{2}} \delta_2 f_c^y \sin \gamma d\gamma \tag{13}$$

where δ_2 represents the distance from the contact point to the instantaneous axis p_{axis} , γ represents the angle from the y-z plane to the helix plane containing the helical body.

In another step in Figure 2c,d where the apex of the deformable helical body touches the bottom of the container, assuming that there is a constant sliding friction coefficient, the resistive friction force can also be expressed as f_c^z and f_c^y . whereas, the distance from the contact point to the instantaneous axis p_{axis} is expressed as δ_1 , which yields,

$$\tau_{c1} = 2 \int_0^{\frac{\pi}{2}} \delta_1 f_c^y \sin \gamma d\gamma \tag{14}$$

Within the two steps in spindle-like rotation locomotion, the total friction resistive torque τ_c can be expressed as,

$$\tau_c = \tau_{c1} + \tau_{c2} \tag{15}$$

The total magnetic force \vec{f}_m and torque $\vec{\tau}_m$ acting on the body can be represented as

$$\begin{cases} \vec{\tau}_m = M \times B\\ \vec{f}_m = (M \cdot \nabla) B \end{cases}$$
(16)

where M is the magnetization vector of the magnetic particle, and B is the magnetic field vector.

The magnetic coils in our lab can only create an uniform rotating magnetic field, so the gradient of the magnetic field is zero and the magnetic force f_m becomes zero. We focus on the dynamic analysis that the helical microswimmer can perform spindle-like rotation locomotion approximately in sync with rotating magnetic field at low actuate frequency. In conclusion, submitting (13), (15) and (16) into (2), and the final dynamic equations can be given by,

$$\begin{bmatrix} a_{11} & a_{12} \\ a_{21} & a_{22} \end{bmatrix} \begin{bmatrix} v \\ f_{act} \end{bmatrix} = \begin{bmatrix} c_1 \\ c_2 \end{bmatrix}$$
(17)

where these following coefficients of the dynamic model can be given by,

$$a_{11} = \sum_{i=1}^{n} \lambda A \sin \beta \left(C_n - C_l \right) \cos \theta_i$$

$$a_{12} = -\sum_{i=1}^{n} \lambda A^2 \left(C_n \cos \beta - C_l \sin \beta \tan \beta \right) \cos \theta_i$$

$$a_{21} = -\sum_{i=1}^{n} \lambda \left(C_n \sin \beta \tan \beta + C_l \cos \beta \right) \cos \theta_i$$

$$a_{22} = \sum_{i=1}^{n} \lambda A \sin \beta \left(C_n - C_l \right) \cos \theta_i$$

$$c_1 = \left(\rho_{lotus} - \rho_{liquid} \right) V_{lotus} g \left(2 \int_0^{\frac{\pi}{2}} \delta_2 f_c^y \sin \gamma d\gamma + 2 \int_0^{\frac{\pi}{2}} \delta_1 f_c^y \sin \gamma d\gamma \right) - MB$$

$$c_2 = f_c^z$$

Then we can get the following equations, which characterized the process of the lotus-root microswimmer spindle-like rotation locomotion on the bottom of the container. Within one locomotion cycle (γ changes from 0° to 360°), the relation between locomotion velocity $v_{forward}$ perpendicular to P_{axis} axis, locomotion velocity v_{side} along P_{axis} axis and frequency is established from (17).

$$f_{act}^{1} = \frac{c_1 a_{21} - c_2 a_{11}}{a_{12} a_{21} - a_{22} a_{11}} \tag{18}$$

$$v_{side} = \frac{c_1 a_{22} - c_2 a_{12}}{a_{22} a_{11} - a_{12} a_{21}} \tag{19}$$

$$v_{forward} = \frac{1}{2} \left[(h_1 - \delta_1) f_{act}^1 + (h_2 - \delta_2) f_{act}^1 \right]$$
(20)

For a rigid helical body, its locomotion velocity is $f_{act}A$ in Figure 1. Because of $\frac{1}{2}[(h_1 - \delta_1) + (h_2 - \delta_2)] > A$, it can be inferred that $v_{forward} > f_{act}A$. Figure 3a shows spindle-like rotation locomotion with an inclination angle ϑ in each step from top view, the left one is one-point-support step, the right one is the zero-point-support step. Figure 3b shows the propulsion force, the propulsion force and the friction force from side view. Experiments find that the helical body is not propelled apart from the bottom of the container. So we can conclude that $v_{side} = 0$ since the propulsion force $f_d \sin \vartheta$ is less than the net gravitational force $(\rho_{lotus} - \rho_{liquid}) V_{lotusg}$.

Micromachines 2017, 8, 349

Based on above discussions, a simplified torque balance equation can be derived in one-point-support step for spindle-like rotation locomotion with an inclination angle ϑ (the right one in Figure 3a),

$$\sum_{i=1}^{n} \left(-\lambda A^2 \left(C_n \cos \beta - C_l \sin \beta \tan \beta \right) f_{act}^4 \cos \theta_i \right) + MB -$$

$$2 \int_0^{\frac{\pi}{2}} f_c \delta_3 \cos \phi d\phi - 2 \int_0^{\frac{\pi}{2}} \mu \left(\rho_{lotus} - \rho_{liquid} \right) V_{lotus} g \left(h_4 - \delta_4 \right) \sin \phi d\phi = 0$$
(21)

where μ_{fric} is the friction coefficient.

$$f_{c} = \mu_{fric} \left(\left(\rho_{lotus} - \rho_{liquid} \right) V_{lotus} g - f_{d} \sin \vartheta$$
$$f_{d} = \sum_{i=1}^{n} \left(\lambda A \sin \beta \left(C_{n} - C_{l} \right) f_{act} \cos \theta_{i} \right)$$

In another step, a simplified torque balance equation can be derived in zero-point-support step for spindle-like rotation locomotion with an inclination angle ϑ (the left one in Figure 3a),

$$\sum_{i=1}^{n} (-\lambda A^2 (C_n \cos \beta - C_l \sin \beta \tan \beta) f_{act}^3 \cos \theta_i) + MB - 2 \int_0^{\frac{\pi}{2}} \mu \left(\rho_{lotus} - \rho_{liquid}\right) V_{lotus} g(h_4 - \delta_3) \sin \varphi d\phi = 0$$
(22)

Then we can get the following equations, which characterized the process of the lotus-root microswimmer spindle-like rotation locomotion with an inclination angle ϑ . f_{act}^4 is derived from (21), f_{act}^3 is derived from (22). Within one locomotion cycle (φ changes from 0° to 360°), the relation between spindle-like rotation locomotion velocity $v_{forward}^i$ perpendicular to P_{axis} axis and frequency is established.

$$f_{act}^{4} = \frac{MB - 2\int_{0}^{\frac{\pi}{2}} f_c \delta_3 \cos\phi d\phi - 2\int_{0}^{\frac{\pi}{2}} \mu \left(\rho_{lotus} - \rho_{liquid}\right) V_{lotus}g \left(h_4 - \delta_4\right) \sin\phi d\phi}{\sum_{i=1}^{n} \left(\lambda A^2 \left(C_n \cos\beta - C_l \sin\beta \tan\beta\right) \cos\theta_i\right)}$$
(23)

$$f_{act}^{3} = \frac{MB - 2\int_{0}^{\frac{\pi}{2}} \mu\left(\rho_{lotus} - \rho_{liquid}\right) V_{lotus}g\left(h_{4} - \delta_{3}\right)\sin\varphi d\phi}{\sum_{i=1}^{n} \left(\lambda A^{2}\left(C_{n}\cos\beta - C_{l}\sin\beta\tan\beta\right)\cos\theta_{i}\right)}$$
(24)

$$v_{forward}^{\vartheta} = \frac{1}{2} \left[(h_4 - \delta_3) f_{act}^3 + (h_4 - \delta_4) f_{act}^4 \right]$$
(25)

where h_4 is the center height from the center position to the end of the helical body, δ_3 is the distance between the apex and the instantaneous axis P_{axis} , δ_4 is the distance between the end and the instantaneous axis P_{axis} . Due to its whole body suspending in liquid for f_{act}^3 , its locomotion velocity $(h_4 - \delta_3) f_{act}^3 = 0$. For a rigid helical body, its spindle-like rotation locomotion velocity is $f_{act}A$ in Figure 1. Because of $\frac{1}{2} (h_4 - \delta_4) > A$, it can be inferred that $v_{forward}^{\vartheta} > f_{act}A$.

3. Experimental Setup and Fabrication of the Helical Microswimmers

The helical microswimmers in this paper are actuated by a 3D Helmholtz coil system shown in Figure 4. The 3D Helmholtz coil system can generate a uniform magnetic field in working space with size of approximately $80 \times 50 \times 40$ mm, drived by 3 Maxon ESCON 70/10 motor drivers (Maxon Motor, Sachseln, Switzerland). PC can send out control signals through Sensoray S826 PCIe A/D IO card to the motor drivers. This system also comes with a single camera (PointGreyGS3-U3-41C6M, FLIR Integrated Imaging Solutions, Inc., Richmond, BC, Canada) mounted on the top of the 3D Helmholtz coils, providing overviews for monitoring. In the experiments, the rotations of the the helical microswimmers can be recorded by the camera. The frame rate is about 50 frames/s. The spindle-like locomotion velocity is measured offline by the traveled distance in pixel per unit time. Then, it is

converted into international unit. The swimming behaviour of the deformable helical microswimmers has not been clearly defined mainly due to the limited fabrication. Moreover, the traditional fabrication process is time-consuming. That is why scaled-up helical swimmers are designed. A simple reproducible method is illustrated in Figure 5a. The helical fibers are mechanically isolated from the roots of lotus. The whole process goes sequentially through cutting, breaking and stretching. We can controll the stretching span D_{span} in Figure 5b and thus tailor the length of the helixes. To enable magnetic acutation, the obtained helixes are subject to the coating of magnetic materials. Then they are diced into the desired lengths. The helical dimensions of the microswimmers, and the overall shape, remain constant throughout the whole fabrication process. The high density of helixes within the lotus-root in Figure 5b provides an ideal platform for easy production of the functional helical microswimmers in Figure 5c. This method is thus extremely promising because it provides a cost-effective and straightforward production of helical magnetic microswimmers and offers substantial savings in material requirements and processing costs compared to the commonly used methods for fabricating helical microswimmers. Employing above methods, we can fabricate three helical microswimmers with different length including 4 mm, 2.3 mm, 1.4 mm and name them LRH4, LRH2 and LRH1 respectively in Figure 5c. Based on the following scanning electron microscopy (SEM) image in Figure 5d, the distribution of magnetic matter (i.e., Fe₃O₄) is relatively-uniform on lotus-root's fiber.

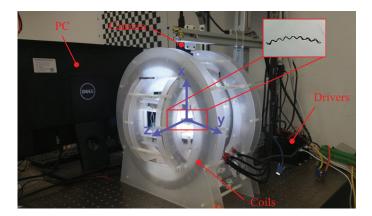


Figure 4. 3D Helmholtz coil system.

The fluid motion around the helical swimmer can be characterized by one dimensionless parameter: the Reynolds numbers. Due to the small scale of E. coli bacteria, its swimming environment can be characterized by low Reynolds numbers. Consequently we select the 12.5% glycerinum solution to simulate the low Reynolds numbers environment. As for the helical microswimmers swimming in the glycerol solution, its density and viscosity in 20 °C are 1.033 g/cm³ and 13 mPa·s, respectively. The locomotion velocity of the helical swimmer is 2–7 mm/s. Therefore, the calculated Reynolds number is approximately 0.16–0.55, the helical swimmer locomotes at low Reynolds numbers.

Here we use element analysis to evaluate the amount of superparamagnetic nanoparticles on a lotus-root's fiber with an energy-dispersive X-ray spectroscopy (EDX) analyzer mounted on the FEI Quanta 400F(FEI Company, Hillsboro, OR, USA) (accelerating voltage at 20 kV). The Fe element is assigned to magnetic coating (Fe₃O₄), C element to the lotus-root's fiber, O element to the magnetic coating and lotus-root's fiber, and Si element to the silicon subtract used to support scanning electron microscope (SEM) samples. According to these data from the EDX analyzer, magnetic coating ratio $\psi = m_{helix}/m_{coating}$ takes about 5.4%, m_{helix} denotes the total mass of the lotus-root's fiber and the magnetic coating layer, $m_{coating}$ denotes the mass of the magnetic coating layer.

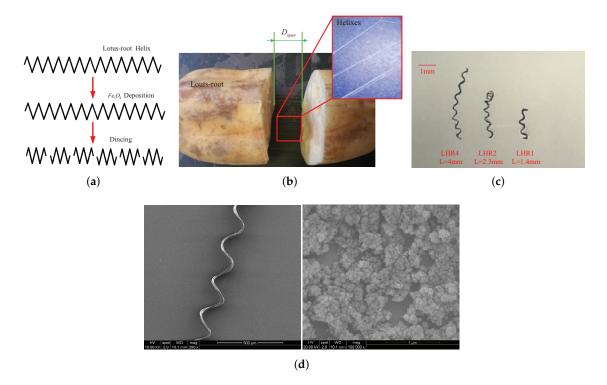


Figure 5. (**a**) Schematic illustrating the steps for the preparation of the lotus-based microswimmers; (**b**) Image illustrating arbitrary stretching of the lotus-root and the isolated helical structure; (**c**) Image of multiple magnetic helical microswimmers from (**a**); (**d**) The left: low-magnification scanning electron microscope (SEM) image of the lotus-root's fiber with magnetic coating. The right: enlarged SEM image of the selected area in the left, showing a relatively-uniform magnetic coating. Field emission scanning electron microscope (FESEM) images were acquired using a FEI Quanta 400F (FEI Company, Hillsboro, OR, USA) microscope with an accelerating voltage of 10 kV.

4. Results and Discussion

4.1. Experiments and Analysis on Spindle-like Rotation Locomotion

The following experiment were carried out to verify the curvature of the helical body under different actuate frequency as well as the relation between the spindle-like locomotion velocity $v_{forward}$, the propulsion velocity v_{side} and the actuate frequency f_{act} . To quantify the curvature, we define the distance D between the apex of the deformable helical body and the end shown in Figure 2a.

Figure 6a illustrates the distance D for LRH4, LRH2, LRH1 in function of the actuate frequency f_{act} for different length of the magnetized helixes. With the increasing of the rotating frequency, the curvature of the bended helical microswimmers will increase a little both in water and in 12.5% glycerinum. So the distance D will shrink a little with the actuate frequency increasing. Taking LRH4 in water for example, the distance decreases from 7 pixels at 1 Hz to 5 pixels at 3 Hz because of the viscous drag force or torque. We also find another characterized variable called "step-out frequency", above the step-out frequency leads to poor propulsion performance. Taking LRH4 and LRH2 in water for example, the step-out frequency is 3 Hz and 1.5 Hz respectively in Figure 6b. The reasons are as follows. $v_{forward}$ in water becomes larger than that in 12.5% glycerinum. Due to the larger viscosity of 12.5% glycerinum compared with water, the calculated frequency f_{act}^1 from (18) may become smaller in 12.5% glycerinum. From Figure 6, the changes D in water and in 12.5% glycerinum is the calculated frequency f_{act}^1 and has nothing to do with the distance D.

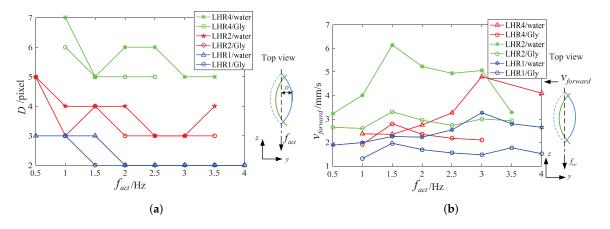


Figure 6. (a) The relation between distance D and actuate frequency f_{act} for different length; (b) The relation between spindle-like locomotion velocity $v_{forward}$ and actuate frequency f_{act} for different length.

During spindle-like rotation locomotion on the bottom of the container, a tiny propulsion velocity v_{side} in Figure 7 has been found but its propulsion performance is poor compared with the $v_{forward}$. Firstly, the reason for the propulsion velocity v_{side} is its helical structure during the non-reciprocating motion. Secondly, the reasons for the tiny propulsion velocity v_{side} are the small helix and low actuate frequency f_{act} . Another interesting phenomenon is that the same lotus-root microswimmer in 12.5% glycerinum has more larger propulsion velocity v_{side} but more smaller step-out frequency. The reason is that the viscosity in 12.5% glycerinum is larger than that in water. Under the step-out frequency, the experiment results show that the viscosity mainly contributes to the larger propulsion velocity v_{side} in spite of the smaller calculated frequency f_{act}^1 . Above the step-out frequency, the propulsion velocity v_{side} in 12.5% glycerinum to the step-out frequency v_{side} in spite of the smaller calculated frequency f_{act}^1 . Above the step-out frequency, the propulsion velocity v_{side} in 12.5% glycerinum to the time tresults show that the viscosity mainly contributes to the larger propulsion velocity v_{side} in 12.5% glycerinum the time tresults show that the viscosity mainly contributes to the propulsion velocity v_{side} in 12.5% glycerinum drops more heavily than that in water. The experiment results show that the viscosity mainly contributes to the propulsion velocity v_{side} in spite of the bigger calculated frequency f_{act}^1 .

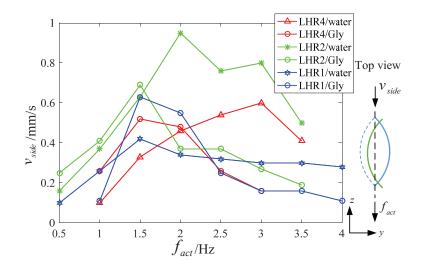


Figure 7. The relation between the propulsion velocity v_{side} and actuate frequency f_{act} for different length.

4.2. Experiments and Analysis on Spindle-Like Rotation Locomotion with an Inclination Angle

In addition, we also focus on another spindle-like rotation locomotion with an inclination angle ϑ and selectively choose 30°, 45°, 60° and 90° to calculate the steering vector. We design a series of experiments to show the relation between the inclination angle ϑ and the actuate frequency f_{act} . By comparing them, we can find relatively stable and fast swimmer mode rotating along decided axis. Figure 8a describes the functional relation between the swim velocity $v_{forward}^{LHR4}$ and the inclination angle ϑ in water. The spindle-like locomotion velocity $v_{forward}^{LHR4}$ is approximatively linear inverse proportional to the inclination angle ϑ both in water and in 12.5% glycerinum. Figure 8b describes the functional relation velocity $v_{forward}^{LHR4}$ and the actuate frequency f_{act} for different inclination angles ϑ in 12.5% glycerinum. It shows that the lotus-root microswimmer locomotes at relative slow velocity compared with that in water. It can be concluded that the higher viscosity leads to lower the spindle-like locomotion velocity $v_{forward}^{LHR4}$.

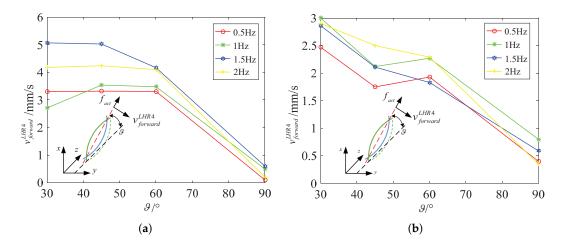


Figure 8. LHR4: the relation between $v_{forward}^{LHR4}$ and the inclination angle ϑ for different actuate frequency $f_{act.}$ (a) In water (b) in 12.5% glycerinum.

Specifically, because of the higher viscosity, the resistance coefficients C_n and C_l increase which leads to an increase of the denominator of f_{act}^3 and f_{act}^4 , and an increase of the propulsion force f_d . Based on analysis of the f_c and f_d , we can make sure that f_{act}^3 decreases a bit, and that f_{act}^4 changes a bit. Although f_{act}^4 may increase or decrease a bit, the experiment results report that the spindle-like locomotion velocity $v_{forward}^{LHR4}$ decreases from in water to in 12.5% glycerinum. So it can be inferred that f_{act}^4 also decreases and slows down the spindle-like locomotion velocity $v_{forward}^{LHR4}$. In Figure 9, the experiment results verify our above conclusion and show another spindle-like rotation locomotion characteristic. Moreover, LHR2 and LHR1 can keep a higher spindle-like locomotion velocity at 45° in water but not in 12.5% glycerinum.

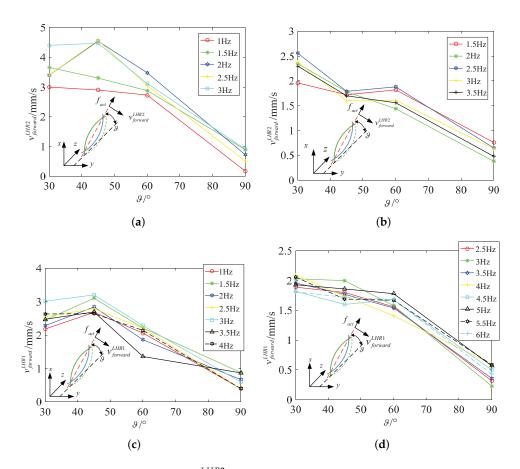


Figure 9. LHR2: the relation between $v_{forward}^{LHR2}$ and the inclination angle for different actuate frequency $f_{act.}$ (**a**) In water (**b**) in 12.5% glycerinum; LHR1: the relation between $v_{forward}^{LHR1}$ and the inclination angle ϑ for different actuate frequency $f_{act.}$ (**c**) In water (**d**) in 12.5% glycerinum.

Figure 10 shows that LRH4 in water can locomote at relative high speed at 45° at four different actuate frequencies, but it can keep stable spindle-like locomotion velocity at 60° at four different actuate frequencies. In 12.5% glycerinum, it can also keep stable spindle-like locomotion velocity at 60° but locomote at relative high speed at 30°. In further analysis, during the process of the inclination angle ϑ increasing from 30° to 90°, f_c decreases in water or in 12.5% glycerinum which makes f_{act}^4 increase a bit. This is approximately in contradiction with the experimental results, but we cannot neglect the parameters ($h_4 - \delta_4$). These two parameters jointly change the spindle-like locomotion. Velocity $v_{forward}^i$. Due to the deformability of the lotus root fibers, the distance ($h_4 - \delta_4$) between the center and rotation instantaneous axis p_{axis} can change during the spindle-like rotation locomotion. For LHR4, it can be determined that the parameter ($h_4 - \delta_4$) reach its maximum at 45° in water, and at 30° in 12.5% glycerinum. Thus Figure 11 shows that LHR4 can keep a higher spindle-like locomotion velocity $v_{forward}^{LHR4}$ at 45° in water, and at 30° in 12.5% glycerinum. In Figure 11, the experiment results verify our above conclusion for LHR2, LHR1. For LHR2, it can keep relative high locomote velocity $v_{forward}^{LHR1}$ at 3 Hz at 45° in water, at 4 Hz at 30° in 12.5% glycerinum.

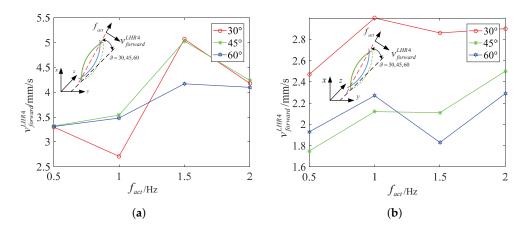


Figure 10. LHR4: the relation between spindle-like rotation locomotion $v_{forward}^{LHR4}$ and actuate frequency f_{act} for different inclination angle ϑ . (a) In water (b) in 12.5% glycerinum.

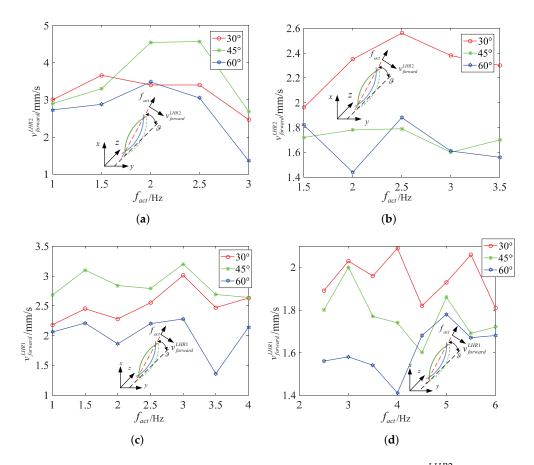


Figure 11. LHR2: the relation between spindle-like locomotion velocity $v_{forward}^{LHR2}$ and actuate frequency f_{act} for different inclination angle. (a) In water (b) in 12.5% glycerinum; LHR1: The relation between spindle-like rolling velocity $v_{forward}^{LHR1}$ and actuate frequency f_{act} for different inclination angle; (c) in water (d) in 12.5% glycerinum.

Figure 12 describes the functional relation between the area S_{LHR4} of the body and the inclination angle ϑ . According to analysis the little change of the area, we can find that the microswimmer can keep its attitude stable at 45° in water, at 45° in 12.5% glycerinum above 0.5 Hz during swimming. The area

 S_{LHR4} changes between 0.96 mm² and 1.05 mm² at 45° in water, and changes between 1.04 mm² and 1.14 mm² at 45° in 12.5% glycerinum.

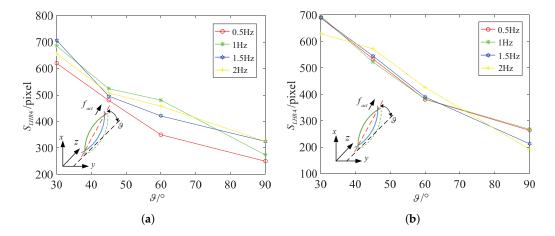
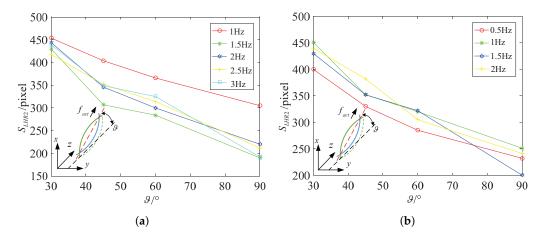


Figure 12. LHR4: the relation between pixel area S_{LHR4} and inclination angle ϑ for different actuate frequency. (a) In water (b) in 12.5% glycerinum.

In similar analysis, we can find that LRH2 can keep its attitude stable above 1 Hz during swimming. Particularly, LRH2 can keep its attitude stable at 45° in water, at 30° in 12.5% glycerinum above 0.5 Hz during swimming, as shown in Figure 13a,b. The area S_{LHR2} of the helical body fluctuates a little at different inclination angles above 1 Hz. The area S_{LHR2} changes between 0.62 mm² and 0.71 mm² at 45° in water not including 1 Hz, and changes between 0.8 mm² and 0.9 mm² at 30° in 12.5% glycerinum. It is sufficient to verify that LRH2 can both swim at relative high speed $v_{forward}^{LHR2}$ and keep its attitude stable at 45° at 2 Hz in water, at 30° at 2 Hz in 12.5% glycerinum.

In Figure 13c,d, we can also find that LRH1 can keep its attitude stable at about 3 Hz during swimming. The area S_{LHR1} changes between 0.116 mm² and 0.12 mm² at 60° in water, and changes between 0.14 mm² and 0.16 mm² at 60° in 12.5% glycerinum. Particularly, LRH1 can keep its attitude stable at 60° in water or in 12.5% glycerinum.



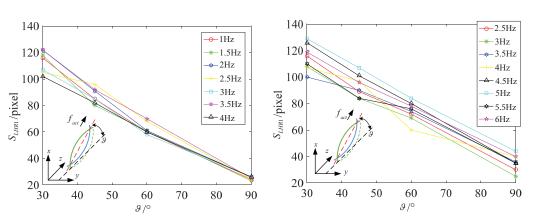


Figure 13. LHR2: the relation between pixel area S_{LHR2} and inclination angle ϑ for different actuate frequency. (a) In water (b) in 12.5% glycerinum; LHR1: the relation between pixel area S_{LHR1} and inclination angle ϑ for different actuate frequency. (c) In water (d) in 12.5% glycerinum.

(d)

4.3. Discussion

(c)

In this section, we select LHR4 (the left one in Figure 14) and a rigid helical microswimmer (RHM) (the right one in Figure 14) to analysis the propulsion performance of the spindle-like rotation locomotion. As for the RHM, the 60% glycerol solution is selected to simulate the low Reynolds numbers. Its density and viscosity in 20 °C are 1.14 g/cm³ and 60 mPa·s, respectively. The locomotion velocity of the helical swimmer is 6–13 mm/s. Therefore, the calculated Reynolds number is approximately 0.17–0.41 which is similar to the low Reynolds number 0.16–0.55 for LHR4. The measured diameter D_{soft} of the helix of the LHR4 is about 0.4 mm and the measured diameter D_{rigid} of the helix of RHM is about 1.5 mm. If the body of LHR4 is rigid, the theoretical locomotion velocity ratio $\chi_1 = v_{rigid} / v_{soft}$ is 3.75 with the same actuate frequency. Nevertheless, the calculated locomotion velocity ratio χ_1 is 2.6. Therefore, it is confidence that the LHR4 with the soft body can locomote faster.

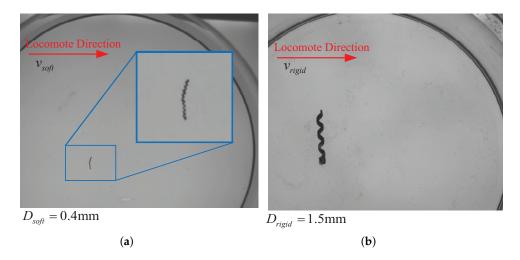


Figure 14. Analysis on propulsion performance at Reynolds number. (a) The LHR4 locomotes along the stright line; (b) the RHM locomotes along the stright line. The calculated locomotion velocity ratio χ_1 decreases to 2.6, so it is confidence that the LHR4 with the soft body can locomote faster.

Due to the heterogeneous distribution of the shrinking stress, the soft helical microswimmers are bent lightely initially for different length. In addition, due to their soft and deformable bodies, they undergo a swimming motion which is a spindle-like rotation locomotion. The propulsion mechanism of the spindle-like rotation locomotion change the equivalent rotation radius from the radius $D_{soft}/2$ to the bigger one δ_1 or δ_2 (see Figure 2b,d). Consequently, the propulsion performance of spindle-like rotation locomotion is better than helical propulsion.

The guideline to make a faster microswimmer is to find out the optimized curvature-length ratio $\chi_2 = D/L$. In this paper, three helical microswimmers with different length including 4 mm, 2.3 mm, 1.4 mm, named LRH4, LRH2 and LRH1 are used in Figure 5c. From Figure 6a, the curvature-length ratio $\chi_{LHR4} \approx 1.25$, $\chi_{LHR2} \approx 1.3$ and $\chi_{LHR1} \approx 1.42$ can be calculated when actuate frequency $f_{act} > 1.5$ Hz. From Figure 6b, we can LRH2 locomotes faster than others both in water and 12.5% glycerinum when actuate frequency $f_{act} > 1.5$ Hz. To obtain better propulsion performance of the fabricated microswimmers, it is better to keep the curvature-length ratio χ_2 within 1.25 and 1.42.

5. Conclusions

In conclusion, we present a lotus-root-based magnetically propelled helical microswimmer, which is fabricated from the fiber of lotus-root coated with magnetic nanoparticles. This fabrication method is easy to achieve at low cost. The new helical microswimmers are fabricated by the simple coating of lotus-root-based fibers with a thin magnetic layer. As the fiber of lotus-root with magnetic coating is deformable, the microswimmers show an attracting spindle-like rotation locomotion actuated by the uniform rotate magnetic field. Spindle-like rotation locomotion in water or in 12.5% glycerinum is analyzed in detail. By modeling its dynamical model in spindle-like rotation locomotion and spindle-like rotation locomotion with an inclination angle, we have established the relation between the spindle-like locomotion velocity and the actuate frequency respectively. we find out that the curvature of the shape decreases as a function of actuate frequency, which is related to the deformability of lotus-root fibers, and that the microswimmer can locomote faster than that with rigid body in both experiments actuated by uniform rotate magnetic field. In addition, the viscosity is proved to have a great impact on the spindle-like locomotion velocity. Specifically, the higher the viscosity is in 12.5% glycerinum, the lower $v_{forward}$ is in spindle-like locomotion and spindle-like locomotion with an inclination angle, but the higher v_{side} becomes in spindle-like locomotion. In the future, a closed-loop visual servo control algorithm will be employed and the steer characteristics will be analyzed in spindle-like rotation locomotion and spindle-like rotation locomotion with an inclination angle.

Acknowledgments: This work was supported by the National Natural Science Funds of China for Young Scholar with the Project No. 61703392, the Science, Technology and Innovation Committee of Shenzhen Municipality (SZSTI) Basic Research Fund Project (No. JCYJ20160408152617408) and Fundamental Research and Discipline Layout project (No. JCYJ20170413152640731).

Author Contributions: Jia Liu made the main contribution on literature review, led the development of the paper and carried on the experiments by the direction of Tiantian Xu and Xinyu Wu. Yanming Guan, Xiaohui Yan and Chengwei Ye performed supports and discussions. All authors reviewed and approved the submitted paper.

Conflicts of Interest: The authors declare no conflict of interests.

References

- Nelson, B.; Kaliakatsos, I.; Abbott, J. Microrobots for minimally invasive medicine. *Annu. Rev. Biomed. Eng.* 2010, 12, 55–85.
- Tottori, S.; Zhang, L.; Qiu, F.; Krawczyk, K.; Franco-Obregon, A.; Nelson, B. Magnetic helical micromachines: Fabrication, controlled swimming, and cargo transport. *Adv. Mater.* 2012, 24, 811–816.
- 3. Qiu, F.; Mhanna, R.; Zhang, L.; Ding, Y.; Fujita, S.; Nelson, B. Artificial bacterial flagella functionalized with temperature-sensitive liposomes for controlled release. *Sens. Actuators B Chem.* **2014**, *196*, 676–681.
- 4. Fischer. P.; Ghosh, A. Magnetically actuated propulsion at low Reynolds numbers: Towards nanoscale control. *Nanoscale* **2011**, *3*, 557–563.

- 5. Hosseinidoust, Z.; Mostaghaci, B.; Yasa, O.; Park, B.; Singh, A.; Sitti, M. Bioengineered and biohybrid bacteria-based systems for drug delivery. *Adv. Drug Deliv. Rev.* **2016**, *106*, 27–44.
- 6. Park, B.; Zhuang, J.; Yasa, O.; Sitti, M. Multifunctional bacteria-driven microswimmers for targeted active drug delivery. *ACS Nano* 2017, *11*, 8910–8923.
- 7. Stanton, M.; Park, B.; Vilela, D.; Bente, K.; Faivre, D.; Sitti, M. Magnetotactic bacteria powered biohybrids target *E. Coli* biofilms. *ACS Nano* **2017**, *11*, 9968–9978.
- 8. Li, J.; Gao, W.; Zhang, L.; Wang, J. Micro/nanorobots for biomedicine: Delivery, surgery, sensing, and detoxification. *Sci. Robot.* **2017**, *2*, eaam6431.
- 9. Peyer, K.; Zhang, L.; Nelson, B. Bio-inspired magnetic swimming microrobots for biomedical applications. *Nanoscale* **2013**, *5*, 1259–1272.
- 10. Peyer, K.; Tottori, S.; Qiu, F.; Zhang, L.; Nelson, B. Magnetic helical micromachines. *Chem. A Eur. J.* **2013**, 19, 28–38.
- 11. Khalil, I.; Tabak, A.; Sadek, K.; Mahdy, D.; Hamdi, N.; Sitti, M. Rubbing against blood clots using helical robots: Modeling and in vitro experimental validation. *IEEE Robot. Autom. Lett.* **2017**, *2*, 927–934.
- 12. Zhang H.; Hutmacher, D.; Chollet, F.; Poo, A.; Burdet, E. Microrobotics and MEMS based fabrication techniques for scaffold based tissue engineering. *Macromol. Biosci.* **2005**, *5*, 477–489.
- 13. Zhang, L.; Peyer, K.; Nelson, B. Artificial bacterial flagella for micromanipulation. *Lab Chip* **2010**, *10*, 2203–2215.
- 14. Huang, T.; Qiu, F.; Tung, H.; Peyer, K.; Shamsudhin, N.; Pokki, J.; Sakar, M.S. Cooperative manipulation and transport of microobjects using multiple helical microcarriers. *RSC Adv.* **2014**, *4*, 26771–26776.
- 15. Peyer, K.; Zhang, L.; Nelson, B. Localized non-contact manipulation using artificial bacterial flagella. *Appl. Phys. Lett.* **2011**, *99*, 174101.
- 16. Purcell, E.M. Life at low Reynolds number. Am. J. Phys. 1977, 45, 3–11.
- 17. Purcell, E. The efficiency of propulsion by a rotating flagellum. Proc. Natl. Acad. Sci. USA 1997, 94, 11307–11311.
- 18. Qiu, T.; Lee, T.; Mark, A.; Morozov, K.; Munster, R.; Mierka, O.; Fischer, P. Swimming by reciprocal motion at low Reynolds number. *Nat. Commun.* **2014**, *5*, 5119–5119.
- 19. Tottori, S.; Nelson, B. Artificial helical microswimmers with mastigoneme-inspired appendages. *Biomicrofluidics* **2013**, *7*, 061101.
- 20. Tabak, A.; Yesilyurt, S. Improved kinematic models for two-link helical micro/nanoswimmers. *IEEE Trans. Robot.* **2014**, *30*, 14–25.
- Erman, A.; Tabak, A. Resistive force theory based modeling and simulation of surface contact for swimming helical micro robots with channel flow. In Proceedings of the 2014 IEEE/ASME International Conference on Advanced Intelligent Mechatronics (AIM), Besacon, France, 8–11 July 2014; pp. 390–395.
- 22. Nourmohammadi, H.; Keighobadi, J.; Bahrami, M. Design, dynamic modelling and control of a bio-inspired helical swimming microrobot with three-dimensional manoeuvring. *Trans. Inst. Meas. Control* **2016**, *1*, 1–10.
- 23. Mahoney, A.; Sarrazin, J.; Bamberg, E.; Abbott, J.J. Velocity control with gravity compensation for magnetic helical microswimmers. *Adv. Robot.* **2011**, *25*, 1007–1028.
- 24. Xu, T.; Hwang, G.; Andreff, N.; Régnier, S. Modeling and swimming property characterizations of scaled-up helical microswimmers. *IEEE/ASME Trans. Mechatron.* **2014**, *19*, 1069–1079.
- 25. Xu, T.; Hwang, G.; Andreff, N.; Régnier, S. Planar path following of 3-D steering scaled-up helical microswimmers. *IEEE Trans. Robot.* 2015, *31*, 117–127.
- 26. Zhang, L.; Abbott, J.; Dong, L.; Kratochvil, B.; Bell, D.; Nelson, B. Artificial bacterial flagella: Fabrication and magnetic control. *Appl. Phys. Lett.* **2009**, *94*, 064107.
- 27. Tottori, S.; Zhang, L.; Peyer, K.; Nelson, B.J. Assembly, disassembly, and anomalous propulsion of microscopic helices. *Nano Lett.* **2013**, *13*, 4263–4268.
- 28. Schamel, D.; Mark, A.; Gibbs, J.; Miksch, C.; Morozov, K.; Leshansky, A.; Fischer, P. Nanopropellers and Their Actuation in Complex Viscoelastic Media. *ACS Nano* **2014**, *8*, 8794–8801.
- 29. Walker, D.; Kubler, M.; Morozov, K.; Fischer, P.; Leshansky, A. Optimal length of low reynolds number nanopropellers. *Nano Lett.* **2015**, *15*, 4412–4416.
- 30. Xu, T.; Hwang, G.; Andreff, N.; Régnier, S. Influence of geometry on swimming performance of helical swimmers using doe. *J. Micro-Bio Robot.* **2016**, *11*, 57–66.
- 31. Qiu, F.; Fujita, S.; Mhanna, R.; Zhang, L.; Simona, B.; Nelson, B. Magnetic helical microswimmers functionalized with lipoplexes for targeted gene delivery. *Adv. Funct. Mater.* **2015**, *25*, 1666–1671.

- 32. Ghosh, A.; Fischer, P. Controlled propulsion of artificial magnetic nanostructured propellers. *Nano Lett.* 2009, *9*, 2243–2245.
- 33. Qiu, F.; Zhang, L.; Peyer, K.; Casarosa, M.; Francoobregon, A.; Choi, H.; Nelson, B. Noncytotoxic artificial bacterial flagella fabricated from biocompatible ORMOCOMP and iron coating. *J. Mater. Chem. B* **2013**, *2*, 357–362.
- Xu, T.; Yu, H.; Zhang, H.; Vong, C.I.; Zhang, L. Morphologies and swimming characteristics of rotating magnetic swimmers with soft tails at low Reynolds numbers. In Proceedings of the 2015 IEEE/RSJ International Conference on Intelligent Robots and Systems (IROS), Hamburg, Germany, 28 September–2 October 2015; pp. 1385–1390.
- 35. Stanton, M.; Park, B.; Miguel, L.; Ma, X.; Sitti, M.; Sánchez, S. Biohybrid microtube swimmers driven by single captured bacteria. *Small* **2017**, *13*, 1603679.
- 36. Li, J.; Sattayasamitsathit, S.; Dong, R.; Gao, W.; Tam, R.; Feng, X. Template electrosynthesis of tailored-made helical nanoswimmers. *Nanoscale* **2014**, *6*, 9415–9420.
- 37. Li, J.; Li, T.; Xu, T.; Kiristi, M.; Liu, W.; Wu, Z. Magneto-acoustic hybrid nanomotor. *Nano Lett.* **2015**, *15*, 4814–4821.
- 38. Sitti, M.; Ceylan, H.; Hu, W.; Turan, M.; Yim, S.; Diller, E. Biomedical applications of untethered mobile milli/microrobots. *Proc. IEEE* 2015, *103*, 205–224.
- 39. Gao, W.; Feng, X.; Pei, A.; Kane, C.; Tam, R.; Hennessy, C.; Wang, J. Bioinspired helical microswimmers based on vascular plants. *Nano Lett.* **2013**, *14*, 305–310.
- 40. Yan, X.; Zhou, Q.; Yu, J.; Xu, T.; Deng, Y.; Tang, T.; Feng, Q.; Bian, L.; Zhang, Y.; Ferreira, A.; et al. Magnetite nanostructured porous hollow helical microswimmers for targeted delivery. *Adv. Funct. Mater.* **2015**, *25*, 5333–5342.
- 41. Hancock, G. The self-propulsion of microscopic organisms through liquids. In *Proceedings of the Royal Society of London A: Mathematical, Physical and Engineering Sciences;* Royal Society: London, UK, 1953; Volume 217, pp. 96–121.
- 42. Brennen, C.; Winet, H. Fluid mechanics of propulsion by cilia and flagella. *Annu. Rev. Fluid Mech.* **1977**, *9*, 339–398.
- 43. Smith, E.; Makarov, D.; Sanchez, S.; Fomin, V.; Schmidt, O. Magnetic microhelix coil structures. *Phys. Rev. Lett.* **2011**, 107, 097204.



© 2017 by the authors. Licensee MDPI, Basel, Switzerland. This article is an open access article distributed under the terms and conditions of the Creative Commons Attribution (CC BY) license (http://creativecommons.org/licenses/by/4.0/).