



# Article Comparing Multi-Objective Local Search Algorithms for the Beam Angle Selection Problem

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Abstract: In intensity-modulated radiation therapy, treatment planners aim to irradiate the tumour according to a medical prescription while sparing surrounding organs at risk as much as possible. Although this problem is inherently a multi-objective optimisation (MO) problem, most of the models in the literature are single-objective ones. For this reason, a large number of single-objective algorithms have been proposed in the literature to solve such single-objective models rather than multi-objective ones. Further, a difficulty that one has to face when solving the MO version of the problem is that the algorithms take too long before converging to a set of (approximately) non-dominated points. In this paper, we propose and compare three different strategies, namely random PLS (rPLS), judgementfunction-guided PLS (jPLS) and neighbour-first PLS (nPLS), to accelerate a previously proposed Pareto local search (PLS) algorithm to solve the beam angle selection problem in IMRT. A distinctive feature of these strategies when compared to the PLS algorithms in the literature is that they do not evaluate their entire neighbourhood before performing the dominance analysis. The rPLS algorithm randomly chooses the next non-dominated solution in the archive and it is used as a baseline for the other implemented algorithms. The jPLS algorithm first chooses the non-dominated solution in the archive that has the best objective function value. Finally, the nPLS algorithm first chooses the solutions that are within the neighbourhood of the current solution. All these strategies prevent us from evaluating a large set of BACs, without any major impairment in the obtained solutions' quality. We apply our algorithms to a prostate case and compare the obtained results to those obtained by the PLS from the literature. The results show that algorithms proposed in this paper reach a similar performance than PLS and require fewer function evaluations.

**Keywords:** multi-objective beam angle optimisation; matheuristic; intensity modulated radiation therapy; Pareto local search

# 1. Introduction

Intensity-modulated radiation therapy (IMRT) is one of the most common techniques in cancer treatment. It aims to eradicate tumour cells by irradiating the tumour region without compromising surrounding normal tissue and organs at risk (OARs). Unfortunately, because of the physics of radiation delivery, there is a trade-off between tumour control and sparing OARs [1,2].

The IMRT planning problem is a complex problem usually split into three subproblems: the beam angle optimisation (BAO), the fluence map optimisation (FMO), and multi-leaf collimator sequencing [1,2]. In the BAO problem, we look for a *beam angle configuration* (BAC), that is, a set of beam angles we will irradiate from. Then, in the FMO problem, the best possible fluence of radiation (according to some optimisation model) for each beam angle in the BAC is computed. Finally, a sequencing problem needs to be solved to control the movement of the multi-leaf collimator leaves during delivery of the optimised fluence [1,3]. It is clear from the process above that selecting high-quality BAC(s) will allow us to obtain better treatment plans during the computation of the FMO problem. In this



Citation: Cabrera-Guerrero, G.; Lagos, C. Comparing Multi-Objective Local Search Algorithms for the Beam Angle Selection Problem. *Mathematics* **2022**, *10*, 159. https://doi.org/10.3390/ math10010159

Academic Editor: David Greiner

Received: 23 November 2021 Accepted: 29 December 2021 Published: 5 January 2022

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**Copyright:** © 2022 by the authors. Licensee MDPI, Basel, Switzerland. This article is an open access article distributed under the terms and conditions of the Creative Commons Attribution (CC BY) license (https:// creativecommons.org/licenses/by/ 4.0/). study, we focus on the problem of selecting a set of beam angles to produce high-quality treatment plans, while ignoring the MLC problem.

In radiation therapy practice, treatment planners usually define the BAC manually in a trial-and-error procedure, mainly driven by their experience and intuition and considering some geometrical features of the problem. Unfortunately, according to several authors from the literature, manual selection may lead to sub-optimal fluence maps [2,4–7].

In the next paragraphs, we shall describe the mathematical model of the MO-BAO problem. Most of the notation we use here was obtained from [1,2,8]: Let *K* be the set of all possible beam angles around the patient. In this work, we consider  $K = \{k\pi/36 : k = 0, 1, 2, ..., 72\}$ . Let  $\mathscr{A} \in \mathscr{P}^N(K)$  be a feasible BAC where  $\mathscr{P}^N(K)$  is the set of all *N*-element subsets of *K*, with N > 0 being the a priori determined number of angles. We denote the *i*-th angle of  $\mathscr{A}$  by  $\mathscr{A}_i$  for i = 1, ..., N. Thus, for a fixed BAC  $\mathscr{A} \in \mathscr{P}^N(K)$ , the general MO-FMO problem can be formulated as

$$f(\mathscr{A}) = \min_{x \in X(\mathscr{A})} z(x), \tag{1}$$

where  $z(x) \in \mathbb{R}^{|R|}$  is a vector of |R| objective functions  $z_r$ , r = 1, ..., |R| and |R| is the total number of regions considered in the problem. Unlike in single-objective formulations, which require the determination of a single optimal fluence map, the solution to this multi-objective problem is a set  $X_E^{\mathscr{A}}$  containing efficient fluence maps of MO-FMO problem (1). We define  $Y_N^{\mathscr{A}} = f(\mathscr{A})$  as the set of associated non-dominated points given by  $Y_N^{\mathscr{A}} = \{z(x) \text{ for all } x \in X_E^{\mathscr{A}}\}.$ 

The MO-BAO problem we are investigating in this paper is

$$\min_{\mathscr{A}\in\mathcal{P}^{N}(K)}\min_{x\in X(\mathscr{A})}z(x),$$
(2)

the solution of which is the set  $A_E$  which contains all efficient BACs which use exactly N angles. A BAC  $\mathscr{A}$  is efficient if  $X(\mathscr{A}) \cap X_E \neq \{\}$ , or equivalently if there is a fluence map  $x \in X(\mathscr{A})$  such that there is no BAC  $\mathscr{B}$  and fluence map  $x' \in X(\mathscr{B})$  with  $z(x') \leq z(x)$ . Additionally, the MO-BAO problem in (2) asks for the generation of a set  $X_E$  containing the efficient fluence maps which belong to those efficient BACs and that lead to the set  $Y_N = \{z(x) : x \in X_E\}$ , the associated set of all non-dominated points. We also write problem (2) as

$$\min_{\mathscr{A}\in\mathcal{P}^{N}(K)}f(\mathscr{A}),\tag{3}$$

to show that solving the MO-BAO problem requires us to also solve the MO-FMO problem (1) for different BACs  $\mathscr{A} \in \mathcal{P}^N(K)$ .

From the formulations above, it is easy to see that from, let us say, a five-beam BAC, we can generate 72 available beams (a typical prostate case), which is an enormous number. Therefore, it is simply not possible to approach this problem using enumeration strategies. Additionally, as reported in [9], state-of-the-art non-linear solvers, such as Knitro and Ipopt, can solve the BAO problem in a clinically acceptable time, with up to 12 available beams. Therefore, the LS algorithms proposed in this paper will only find a set  $\hat{A}_E \subseteq \mathcal{P}^N(K)$  that approximates the actual set of efficient BACs  $\mathcal{A}_E$ . Similarly,  $\hat{X}_E \subseteq X$  will denote the approximation to the set of all the efficient fluence maps  $X_E$ . Images of solutions  $x \in \hat{X}_E$  are denoted by  $y \in \hat{Y}_N$  [2].

We also need to highlight the differences between the MO-BAO problem and the single-objective BAO problem. The main difference between these two problems is the number of solutions we are looking for. While for the MO-BAO problem we generate a set of approximately efficient BACs  $\hat{A}_E$  for the treatment planners we can choose from, in the single-objective BAO problem, we only generate one optimal BAC, which is presented as the "best" one. This difference in the number of generated solutions is important as several clinical considerations cannot be included in the mathematical model. Thus, offering a set of (hopefully) diverse BACs allows treatment planners to compare different treatment

plans considering the objective function values and also the clinical considerations that are not explicitly included in the model.

The remainder of this paper is as follows: Section 2 presents the IMRT problem focusing on the MO-BAO problem. We also present in this section the mathematical model that will be used in this study. In Section 3, we present a brief literature review and then the MO-BAO model considered in this paper is introduced. Then, in Section 4, the implemented Pareto local search strategies are outlined. In Section 5, we describe the instances we use in this study and discuss the results obtained for each algorithm. Finally, we draw some conclusions in Section 6 as well as outline future research lines.

# 2. An Overview of IMRT Optimisation Problems

In IMRT, vector  $x \in \mathbb{R}^n$  denotes a fluence map with *n* beamlets, where the element  $x_i \ge 0$  is the fluence at the *i*-th beamlet. Further, each organ is divided into *voxels*. The radiation dose each voxel *j* receives at each region by fluence map *x* is given by Equation (4) [1].

$$d_j^R(x) = \sum_{i=1}^n A_{ji}^R x_i \text{ for all } j = 1, 2, ..., m^R,$$
(4)

where  $R = \{O_1, ..., O_Q, T\}$  is the index set of regions, T is the index of the tumour and the organs at risk and  $O_q$  with q = 1, ..., Q is the index of the normal tissue. Region R has a total of  $m^R$  voxels indexed by j. The elements of vector  $d^R \in \mathbb{R}^{m^R}$   $(d_j^R)$ , give the total dose delivered to voxel j in region R by the fluence map  $x \in X(\mathscr{A})$ . Here, the dose deposition matrix  $A^R \in \mathbb{R}^{m^R \times n}$  is a given matrix where  $A_{ji}^R \ge 0$  defines the rate at which the radiation dose along beamlet i is deposited into voxel j in region R [1,2].

Given a BAC, several mathematical models for the FMO problem have been proposed in the literature based on the dose distribution in Formula (4). In this paper, we extend a single-objective formulation based on the well-known biological model called *gEUD* to solve the MO-BAO problem. This *gEUD*-based MO-BAO model is briefly introduced in Section 2.1.

#### 2.1. gEUD-Based MO-BAO: Mathematical Formulation

Introduced by [10], the *gEUD* is the biologically equivalent dose that, if delivered uniformly, would lead to the same response as the actual non-uniform dose distribution [10]. The *gEUD* penalises less (more) irradiated voxels in tumour (OAR) regions which leads to a more homogeneous dose distribution in the tumour and the avoidance of overdosed voxels in OARs [2,11–15].

The mathematical expression for *gEUD* is

$$gEUD^{R}(x) = \left(\frac{1}{m^{R}} \sum_{j=1}^{m^{R}} (d_{j}^{R}(x))^{a^{R}}\right)^{1/a^{R}},$$
(5)

where  $a^R$  is a region-dependent parameter and  $d_j^R(x)$  comes from Equation (4). While for the tumour region we will set  $a^R < 0$ , for the organs at risk we make  $a^R > 1$ .

As mentioned in Section 2, the *gEUD*-based model in Equation (6) is considered in this paper to solve the MO-FMO problem in Equation (1). This model has been previously used in [2,3,8,9,16].

$$\begin{array}{ll} \max & gEUD^{T}(x) & (6) \\ \min & gEUD^{O_{q}}(x) & \text{for } q = 1, \dots, Q, \\ \text{s.t.} & x \in X(\mathscr{A}), \end{array}$$

where  $X(\mathscr{A})$  is, again, the set of feasible fluence maps which is defined by  $x \ge 0$  and beamlets  $x_i = 0$  for all beamlets not belonging to beam angles in  $\mathscr{A}$ .

As explained in Cabrera G. et al. [17], the model in (6) can be rewritten as

$$\min_{q} gEUD^{O_q}(x) \qquad \text{for } q = 1, \dots, Q,$$
s.t.  $gEUD^T(x) \ge T^T,$ 
 $x \in X(\mathscr{A}),$ 
(7)

where  $T^T$  is equal to the prescribed *gEUD* of the tumour. The model in Equation (7) allows us to reduce the dimension of the problem from p to p - 1 objective functions without losing a single efficient solution of the original *p*-objectives problem. Further, an infinite number of efficient solutions located on a finite number of rays can be generated using this *gEUD*-based model, each of which corresponds to an efficient solution of the reduced p - 1 objective problem [17]. Thus, the associated *gEUD*-based MO-BAO problem is the minimisation of (7) overall  $\mathscr{A} \in \mathcal{P}^N(K)$ , and can be restated as follows.

$$\min_{\mathscr{A}\in\mathcal{P}^{N}(K)}f_{O_{q}}(\mathscr{A}) = \min_{\mathscr{A}\in\mathcal{P}^{N}(K)}\min_{x\in X(\mathscr{A}):gEUD^{T}(x)\geqq T^{T}}gEUD^{O_{q}}(x) \text{ for } q = 1,\ldots,Q.$$
(8)

It is important to note that the model in (7) is convex and, thus, using scalarisation methods allows us to obtain the set of efficient solutions of these problems. Moreover, it is well known that generating many points for each evaluated BAC is not possible. Thus, in this paper, a comparison between two BACs is made by checking the dominance relationship between their corresponding *sample points* (see [2,8] for a more detailed explanation on sample points). Thus, we will say that a BAC  $\mathscr{A}$  is considered better than BAC  $\mathscr{B}$  if sample point  $s_{\mathscr{A}} \in Y_N^{\mathscr{A}}$  dominates  $s_{\mathscr{B}} \in Y_N^{\mathscr{A}}$  and vice versa. If neither sample point from BAC  $\mathscr{A}$  dominates the sample point belonging to  $\mathscr{B}$  nor the sample point from BAC  $\mathscr{B}$  dominates the one from BAC  $\mathscr{A}$ , we say that the BACs  $\mathscr{A}$  and  $\mathscr{B}$  are incomparable.

As explained in [8], we expect that more useful sample points are obtained if the single-objective function used to generate sample points has a strictly monotone objective function. In this way, we can guarantee that an optimal solution found for the single-objective FMO problem is also an efficient solution of the multi-objective FMO problem in Equation (7) [18]. Then, we use the well-known weighted sum method to compute the sample point of each evaluated BAC. Weights are set up a priori, so all sample points are computed using the same weights. As the weighted sum of the model in Equation (7) is strictly made up of monotone functions, we know that its optimal solutions are also efficient ones. We need to point out that different single-objective functions may lead to different sample points for the same BAC [2]. The considered single-objective weighted sum model (WS) is as follows:

WS: 
$$h(\mathscr{A}) = \min \sum_{q=1}^{Q} \alpha_q g E U D^{O_q}(x)$$
  
s.t.  $g E U D^T(x) \ge e u d_0^T$   
 $\sum_{q=1}^{Q} \alpha_q = 1$   
 $x \in X(\mathscr{A}),$ 
(9)

where  $\alpha_q$  is the importance factor associated with the *q*-th region. Using exact algorithms, the optimal fluence map of a beam angle configuration can be found for the associated weighted sum function. Sample points are then obtained evaluating the optimal solutions of the weighted sum function with the corresponding MO-FMO function (7).

## 3. The Multi-Objective Beam Angle Optimisation Problem

MO-BAO: Literature Review

Despite the inherent trade-off between tumour control and the sparing of OARs, the BAO problem has been mainly tackled from a single-objective point of view. The authors have proposed many strategies where hybrid methods combining exact algorithms and meta-heuristics are the most common. While heuristics seek promising BACs, exact algorithms can compute the optimal solution of the associated FMO problem for a specific BAC. Within this kind of hybrid strategy, we can find genetic algorithms [19–21], particle swarm optimisation [22], ant colony systems [23,24] and simulated annealing [5,25–28]. Local search strategies have also been applied to the single-objective BAO problem [3,16,29–34]. Other methods such as response surface [35], surrogate-based methods [36], guided pattern search [37] and mixed-integer programming approaches [38–40] have also been proposed.

More recently, machine learning methods have also been used for the selection of highquality BACs. For instance, the authors of [41] propose a fast beam orientation selection method based on deep learning neural networks. According to the authors, their approach is as efficient as commercial solvers based on column generation methods. Their approach consists of a supervised DNN trained to mimic a column generation algorithm, which iteratively chooses beam orientations one by one by calculating beam fitness values based on Karush–Kush–Tucker optimality conditions at each iteration [41]. The DNN learns to predict these values and, thus, can make the beam selection faster than the column generation strategy. The same authors in [42] propose a reinforcement learning strategy with a Monte Carlo Tree Search to find high-quality BACs in less time than commercial solvers based on column generation. The reinforcement learning structure guides the MCTS and explores the decision space of beam orientation selection problems. This is achieved based on beam fitness values computed with a previously trained deep neural network. Computed beam fitness values are used to indicate the next best beam to add to the BAC. The authors of [43] propose an approach also based on deep learning to improve the beam selection process. They use a convolutional neural network to identify promising candidate beams by using the radiological features of the patients. They argue that they can predict the influence of a candidate beam on the delivered dose individually and let this prediction guide the selection of candidate beams [43]. The same authors extend their approach to multiple criteria in [44].

The hybrid strategy used to solve the single-objective BAO problem has also been extended to the MO-BAO. In [45], the authors propose a method that combines a MO genetic algorithm, namely NSGAIIc [46] and an FMO solver that uses the well-known Broyden-L-BFGS algorithm. In their approach, each individual's dominance status depends on its fitness, i.e., dominated individuals who have a poor fitness are set to a high-rank value. In contrast, individuals who have a good fitness (non-dominated ones) are set to a low-rank value. Lower-rank individuals are preferred to those with a high-rank value and, thus, they are considered within the next generation with higher probability.

Genetic algorithms have also been considered by Fiege et al. [47]. The authors proposed an algorithm called *Ferret*. The *Ferret* algorithm optimises, simultaneously, the intensity of each beamlet and the beams that are included in a BAC. The authors note that simultaneously solving the BAO and the FMO problems is more challenging as the solution space is highly enlarged. Because of this, and similar to [45], the *Ferret* algorithm uses simplified objective functions in order to speed up the algorithm.

In addition to this, [48] proposed a method called *iCicle*. Unlike the approaches mentioned above, which can be considered as a posteriori methods, the *iCicle* method is an a priori method. That is, the decision-maker preferences are defined before the start of the optimisation, and, therefore, the algorithm ends up with the efficient solution that best suits such preferences. A distinctive feature of the *iCicle* method is that it is a constructive method, i.e., it builds up a solution by adding a beam angle at each iteration. The algorithm stops when adding more beam angles leads to no further improvement in the obtained fluence map. Similarly, in [49], a two-step strategy is introduced. The first step consists of

the calculation of the dose deviation from the prescribed dose, considering the *n*-BAC (a BAC considering *n* beam angles) only. Then, in the second step, beam angles that do not belong to the current *n*-BAC are evaluated based on a score function. The best beam angle, i.e., the one with the best score function value, is added and an (n + 1)-BAC is obtained. One drawback of this kind of method is that the quality of the obtained BAC might depend largely on the quality of the angles selected in early iterations of the algorithm [2]. Readers can find a recent and comprehensive review of multi-criteria approaches for IMRT in [50].

In [2], a first attempt to solve the MO-BAO problem using a single-objective LS is presented. The authors propose an a posteriori method called the two-phase approach to solve the MO-BAO problem. In the first phase, a simple local search algorithm is used to find a locally optimal BAC according to a predefined single-objective function (*sample point*). The local search algorithm is performed several times starting from different initial BACs, resulting in a set of sample points. As mentioned in previous sections, one key feature of sample points is that they are not only optimal but also efficient. That is, for a sample point s = z(x) and  $x \in X(\mathscr{A})$  being the optimal fluence map to the corresponding BAC  $\mathscr{A}$ , there is no fluence map  $x' \in X(\mathscr{A})$  such that  $z(x') \leq z(x)$ . During the second phase, the authors of [2] generate a large set of non-dominated points using the well-known  $\varepsilon$ -constraint method [51,52] and produce a final set of non-dominated points for the treatment planner to choose from [2].

Then, in [8], the natural extension from a single-objective local search to MO local search (MO-LS) is presented. Here, the authors use the two-phase framework proposed in [2], replacing the single-objective local search algorithm with a multi-objective one. While in [2] a BAC is preferred to another based on its single-objective function value, in [8], BACs with a non-dominated samplepoint are kept in the archive, while those BACs with dominated sample points are dropped. Moreover, all the BACs whose sample points resulted in non-dominated points are passed on to the next iteration. Thus, each initial BAC gives rise to a set of sample points in the objective space. The PLS in [8] stops once the set of sample points found are pairwise non-dominated. This set is a set of locally efficient BACs which is passed on to the second phase of the two-phase approach. The second phase of the two-phase approach is the same as in [2]. The same paper [8] also proposes an adaptive PLS, which aims to give more *diversity* to the final set of points. Although the adaptive PLS obtains more and better solutions than the PLS algorithm, it takes too long to find the final set of pairwise non-dominated points. Thus, it is not helpful in clinical practice.

In this paper, we propose three PLS-based algorithms aiming to speed up previously proposed PLS algorithms in [8]. The main difference between the PLS in [8] and the algorithms proposed in this paper is the way we choose the next BAC to be visited among the BACs in the archive. In the original PLS, we enumerate all their neighbours for each BAC in the archive and compute its corresponding sample points. After the sample points of all BACs in the archive have been generated, the dominance analysis is performed. Unlike this, in the algorithms proposed in this paper, we choose only one BAC from the archive, enumerate all its neighbours, compute its corresponding sample points and then perform a dominance analysis within the archive. The fact that, in the proposed algorithms, not all BACs in the archive are being visited before the dominance analysis is performed has two main effects: (i) Some BACs might have never been visited, as their sample point might become dominated before the algorithm chooses them. This means, in general, fewer function evaluations. (ii) The criterion and order we use to choose the next BAC to be visited from the archive become a crucial part of the algorithm, as the path the algorithm follows will depend on this decision.

## 4. Multi-Objective Local Search

In this paper, we implement MO-LS algorithms for the first phase of the two-phase approach of Cabrera-Guerrero et al. [2] to find a set of promising BACs. Although other MO global search methods might be used, we focus on MO-LS algorithms as they provide

solutions that are somehow similar to the ones proposed by practitioners from a geometric point of view, but better in terms of their objective functions values.

Three MO-LS algorithms are implemented and compared to the PLS in [8]. In Section 4.1, the general PLS algorithm is outlined and a brief literature review on PLS is presented for the sake of completeness. Section 4.2 shows the PLS algorithm from [8]. Sections 4.3–4.5 present the PLS variants proposed in this paper.

#### 4.1. Pareto Local Search: General Framework

The Pareto local search (PLS) was independently introduced by Paquete et al. [53] and Angel et al. [54]. PLS is, roughly, the multi-objective extension of the well-known hill-climbing algorithm [55]. The PLS algorithm starts by evaluating an initial solution. For our case, this means we compute the sample point of an initial BAC. Then, given a neighbourhood definition N, a set of BACs within the neighbour of the initial BAC is evaluated. Depending on the neighbourhood definition, we might want to explore the entire neighbourhood instead of only a subset of it. One key difference between PLS algorithms from Paquete et al. [53] and Angel et al. [54] is the way they explore neighbourhoods. We will explain this later in this section.

In single-objective local search algorithms, a current solution is stored at each iteration, and its neighbourhood is explored. Unlike this, in the PLS algorithm, we need to keep an archive of *locally non-dominated sample points* at each iteration. In iteration one, the archive only has the sample point of the initial BAC. Then, we need to update the archive at each iteration, so those sample points that are not dominated by any point in the archive are then added. Finally, those points in the archive that are dominated by those recently generated sample points are removed. That is, at the end of each iteration, the archive contains only non-dominated sample points. This process is repeated until no neighbour sample point is added to the archive.

The decision on how we explore solutions in the archive will depend on the PLS implementation. For instance, [54] proposes a deterministic PLS algorithm where all the solutions in the archive are explored (i.e., its neighbours are evaluated) before a dominance analysis is performed. That is, only once neighbours of all the solutions in the archive have been evaluated is a dominance analysis performed to determine what solutions are removed from (or added to) the archive. Thus, the order used to explore the solutions in the archive has no impact in the final set of locally efficient solutions. Unlike the deterministic algorithm proposed in [54], Paquete et al. [53] propose a stochastic algorithm for which the final set of locally efficient solutions found starting from an initial BAC can be different at each run. This is mainly because the dominance analysis performed over the archive is every time a neighbourhood is explored. Thus, solutions in the archive will depend on the order the archive is explored [55]. Although these original versions of PLS are a straightforward and effective method to solve MO problems, they show a slow convergence [55–57].

In this paper, we aim to accelerate the convergence of the PLS proposed in [53] by implementing three different strategies to choose the next solution to be evaluated. The first strategy is to choose the next solution to be evaluated randomly (rPLS), which is, roughly, the same strategy used in the original algorithm proposed in [53]. The second strategy will be to choose the solution with the best judgement function value (jPLS). The third strategy proposed here favours those solutions that are in the neighbourhood of the last evaluated solution. We call this strategy *neighbours-first* PLS (nPLS). Finally, we compare the obtained results to those obtained by the deterministic PLS from [54]. We explain in detail each implementation in the following sections. These variants of the PLS aim to overcome the convergence issues mentioned before.

All the algorithms above aim to generate a set of locally efficient BACs,  $\mathcal{A}^* \subseteq \hat{\mathcal{A}}_E$ , i.e., BACs for which sample points resulted to be (locally) non-dominated. The set  $\mathcal{A}^*$  is the output of all our PLS-based strategies and it is obtained performing a dominance analysis

over the entire set of sample points computed at each iteration. After the last iteration is performed, only non-dominated sample points remain in the set  $A^*$ .

To generate such a set, our MO-LS algorithms need a neighbourhood  $\mathbb{N}$  to be defined. We use the same neighbourhood for all implemented algorithms. The same neighbourhood definition was also used in [2,8] and it is defined by a  $\pm 5^{\circ}$  in one of the beam angles. Mathematically, the neighbourhood of BAC  $\mathscr{A}$ ,  $\mathbb{N}(\mathscr{A})$ , is defined as follows [8]:

$$\mathcal{N}(\mathscr{A}) = \{\mathscr{B} \in \mathfrak{P}^N(K) : \mathscr{A}_j = \mathscr{B}_j \pm \pi/72 \text{ for some } j = 1 \dots N \text{ and} \\ \mathscr{A}_i = \mathscr{B}_i \text{ for all } i = 1 \dots N, \text{ where } i \neq j \}.$$

Let  $\mathcal{A}^*$  be a set of locally efficient BACs w.r.t. the objective functions in Equation (1). Equivalently, let  $X^*$  be a set containing the corresponding fluence map for each BAC in  $\mathcal{A}^*$ . Fluence maps in  $X^*$  are optimal w.r.t the weighted sum function used to compute the associated sample points. Let  $\mathcal{S}_N = \{z(x) \text{ for all } x \in X^*\}$ , with z being the objective function of the MO-FMO problem in Equation (7), be the set of all non-dominated sample points obtained by the MO-LS algorithms. If two BACs have the same sample point (i.e., the same objective function values), then both points will be considered. Thus, all elements of  $\mathcal{S}_N$  are pairwise non-dominated. It is important to note here that we record only one optimal fluence map for each  $\mathcal{A} \in \mathcal{A}^*$ . Consequently, there is only one sample point in  $\mathcal{S}_N$  for each BAC in  $\mathcal{A}^*$  [2].

#### 4.2. Pareto Local Search

We first try the Pareto Local Search algorithm implemented in [8] which is similar to Angel et al. [54]. The PLS starts with an initial BAC (*initialRandomSolution()* in Algorithm 1), which can be either randomly generated or provided by the treatment planner. The initial BAC is added to the set of locally efficient BACs,  $A^*$ 

Then, the algorithm defines what BACs will be explored next. The way we choose the next neighbour to be explored is a key step of the algorithm as it defines how the algorithm moves through the search space [2]. For the PLS implemented in this paper, the neighbourhood of all the unexplored BACs in  $\mathcal{A}^*$ , denoted by  $\mathcal{A}^*_{unexplored} \subseteq \mathcal{A}^*$ , are explored, i.e., all neighbours of BACs in  $\mathcal{A}^*_{unexplored}$  are evaluated  $(\bigcup_{\mathscr{A}\in\mathcal{A}^*_{unexplored}} \{\mathcal{N}(\mathscr{A})\}$ in Algorithm 1). Each time the neighbourhood of a BAC  $\mathscr{A} \in \mathcal{A}^*_{unexplored}$  is generated, the corresponding BAC  $\mathscr{A}$  is marked as explored and, thus, such a BAC does not longer belong to the set  $\mathcal{A}^*_{unexplored}$ . Sample points of the evaluated BACs are also computed in this step. As explained before, sample points are calculated by solving the weighted sum model in Equation (9).

After this, generated neighbours are added to the set  $\mathcal{A}^*$  and a dominance analysis is performed (*merge()* in Algorithm 1). BACs for which sample points result to be pairwise non-dominated are kept in the set of locally efficient BACs  $\mathcal{A}^*$ . Consequently, BACs that are no longer efficient are removed from  $\mathcal{A}^*$ . The algorithm stops when all BACs in  $\mathcal{A}^*$  have been explored.

The key step in Algorithm 1 is to update  $\mathcal{A}^*$ , that is, to decide what BACs in  $\mathcal{A}^*_{unexplored}$  are considered to be explored in the current iteration. Then, changes in this step will lead to changes in how the algorithm explores the search space. For the standard PLS, we explore the entire neighbourhood of all unexplored BACs, i.e., we explore all BACs in  $\mathcal{A}^*_{unexplored}$ . As a consequence, this algorithm suffers from slow convergence as too many function evaluations are needed, especially if either the neighbourhood size is too large or the set  $\mathcal{A}^*_{unexplored}$  has too many elements. Because we have to solve a complex non-linear problem to evaluate a new BAC, it is essential to avoid unnecessary function evaluations for this problem. We have experimented with three PLS variants that attempt to avoid this inefficiency. For all the three variants, only how  $\mathcal{A}^*$  is updated changes. In the following three sections, we explain how this change is implemented for each algorithm.

#### Algorithm 1: Pareto Local Search.

```
// To generate a set of locally efficient BACs
Input: N (Number of angles in a BAC)
Output: \mathcal{A}^* (Set of locally efficient BACs)
begin
\mathcal{A}^* = \{\}; // \text{ initially empty}
\mathscr{A} = \text{initialRandomSolution}(\mathcal{P}^N(K));
Add \mathscr{A} to \mathcal{A}^*;
repeat
| \mathcal{A}^* = \text{merge}(\mathcal{A}^* \cup \{\cup_{\mathscr{A} \in \mathcal{A}^*: \mathscr{A} \text{ is not explored}} \mathcal{N}(\mathscr{A})\});
until all BACs in \mathcal{A}^* have been explored;
return (\mathcal{A}^*);
end
```

## 4.3. Random Pareto Local Search

The random PLS algorithm (rPLS) differs from the PLS in Algorithm 1 in that, at each iteration, we choose only one BAC  $\mathscr{A} \in \mathscr{A}_{unexplored}^*$  to be explored, i.e., we generate the entire neighbourhood for only one previously unexplored BAC at each iteration.

Then, in the rPLS algorithm, the set  $A^*$  is updated using the following rule:

$$\mathcal{A}^* = \operatorname{merge}(\mathcal{A}^* \cup \{\mathcal{N}(\operatorname{rand}(\mathcal{A}^*_{\operatorname{unexplored}}))\}), \tag{10}$$

where  $rand(\mathcal{A}_{unexplored}^*)$  returns a random element from the set of unexplored BACs. The rPLS algorithm can be obtained by replacing line 6 in Algorithm 1 by the Expression (10).

One advantage of this approach is that it is faster than the PLS introduced before, as it does not explore all the elements in  $\mathcal{A}^*_{unexplored}$  (as PLS does) but instead randomly selects one BAC from the set of unexplored BACs. However, one drawback of the rPLS approach is that it does not exploit problem features, as the decision on the next BAC to be explored is made randomly. The following two approaches overcome this issue and exploit different features of the problem.

## 4.4. Judgement-Function-Guided Pareto Local Search

Just like in the rPLS algorithm, in the judgement-function-guided PLS algorithm (jPLS) only one unexplored BAC  $\mathscr{A} \in \mathcal{A}_{unexplored}^*$  is selected to be explored. Rather than choosing a random BAC to explore next, our jPLS algorithm chooses which of the unexplored BACs  $\mathscr{A} \in \mathcal{A}_{unexplored}^*$  to explore next by estimating their quality by using a *judgement function* [38]  $h(\mathscr{A}) : \mathcal{P}^N(K) \to \mathbb{R}_0^+$ , where smaller values of  $h(\mathscr{A})$  indicate better solutions. This gives an update rule as follows:

$$\mathcal{A}^* = \operatorname{merge}(\mathcal{A}^* \cup \{ \mathcal{N}(\underset{\mathscr{A} \in \mathcal{A}^*_{unexplored}}{\operatorname{arg\,min}} \{h(\mathscr{A})\}) \}), \tag{11}$$

We assume that arg min{} will always return only one BAC. In case two, BACs have the same judgement function value, and only one of them is explored. The jPLS algorithm can be obtained by replacing line 6 in Algorithm 1 by Expression (11).

In our experiments, we consider the weighted sum model in Equation (9) as our judgement function. Thus, in this algorithm, a problem-specific feature (judgement function value) is exploited, and (as we will see in the results) the path followed by the algorithm is greatly influenced by such a judgement function.

#### 4.5. Neighbours-First Pareto Local Search

In the neighbours-first PLS (nPLS) algorithm, we also consider only one unexplored BAC  $\mathscr{A} \in \mathcal{A}^*_{unexplored}$  to be explored, just as in the jPLS and rPLS algorithms introduced

before. However, our nPLS algorithm is different in that we need to maintain both the set of locally optimal BACs  $A^*$  and the last explored solution  $\mathscr{A}$ , which we call the *current solution*. Given this, the update rule for the set  $A^*$  is as follows

$$\mathcal{A}^{*} = \begin{array}{c} \operatorname{merge}(\mathcal{A}^{*} \cup \{\mathcal{N}(rand(\mathscr{A}' \in \{\mathcal{N}(\mathscr{A}) \cap \mathcal{A}^{*}_{unexplored}\}))\}) & \text{if } \mathcal{N}(\mathscr{A}) \cap \mathcal{A}^{*}_{unexplored} \neq \emptyset \\ \operatorname{merge}(\mathcal{A}^{*} \cup \{\mathcal{N}(rand(\mathscr{A} \in \mathcal{A}^{*}_{unexplored}))\}) & \text{otherwise} \end{array}$$
(12)

The nPLS algorithm can be obtained, then, by replacing line 6 in Algorithm 1 by the expression in (12).

The nPLS algorithm's idea is to better explore neighbourhoods by favouring those unexplored BACs that are neighbours of the current solution.

Table 1 summarises the main features of each algorithm. In addition, we include in this table two single-objective local search algorithms, namely the steepest descent and the next descent [3] that we use to compare our MO-LS algorithms.

No Neighbour MO Dominance All Iteration **Next Solution** Meets the Termination Neighbours Analysis per or Consists on Selection Criterion to Be Criterion SO Explored Iteration Chosen Exploring the The neighbourentire hood of all the neighbourhood of No choosing solutions in the PLS MO Υ Υ all solutions in Algorithm ends criterion needed set of NDPs has the set of already been non-dominated explored points (NDPs). If no neighbour Selecting the has a better solution with the objective function best The neighbour-Solution with the value than the hood of all the single-objective hest current solution, function value solutions in the **jPLS** MO Υ Υ single-objective it chooses the within the set of set of NDPs has function value in solution with the NDPs and already been the set of NDPs best objective exploring its explored function value entire from the set of neighbourhood. **NDPs** Randomly The neighbourselecting a hood of all the solution within Randomly among solutions in the rPLS MO Υ Υ the set of NDPs those solutions in Algorithm ends set of NDPs has and exploring its the set of NDPs already been entire explored neighbourhood. Selecting a solution within If no neighbour The neighbourthe set of NDPs dominates the hood of all the First neighbour that dominates current solution, that dominates solutions in the nPLS MO Υ Υ the current it chooses one the current set of NDPs has solution and solution solution. already been randomly from exploring its explored the set of NDPs entire neighbourhood.

Table 1. Algorithm features.

#### 4.6. Second Phase: Exact Optimisation of the MO-FMO Problem

The second phase of our approach is the same as in [2] which, in turn, makes use of (the improved) strategy introduced in [9]. In this phase, detailed in Algorithm 2, the associated MO-FMO is solved for each of the locally efficient BACs found in Phase 1. In [2], the majority of the locally optimal BACs found by the single-objective LS algorithm are not passed onto phase two of the two-phase approach. This is because their sample points are dominated by sample points belonging to other locally optimal BACs. Unlike this, when using MO-LS algorithms, we know that the sample points corresponding to the entire set of locally efficient BACs are non-dominated and, therefore, they all are passed onto phase two.

The goal of the second phase is to find a set of BACs  $\hat{A}_E \subseteq A^*$  that approximates the actual set of efficient BACs  $A_E$  [2].

As Algorithm 2 shows, we need, firstly, to generate a large set  $X_E^{\mathscr{A}}$  of efficient fluence maps of the MO-FMO problem in (7) for each BAC  $\mathscr{A} \in \mathcal{A}^*[2]$ . To achieve this, we can use any scalarisation method such as the  $\varepsilon$ -constraint method [52] (the one used in this paper) or the adaptive  $\varepsilon$ -constraint method [58] (*SolveMO-FMO*() method in Algorithm 2). At each iteration, we merge the set  $X_E^{\mathscr{A}}$  and the initially empty set of (approximately) efficient fluence maps  $\hat{X}_E$  (*merge*()) method in Algorithm 2) by eliminating those fluence maps that are dominated by another one in the union of the sets to be merged. After we merge these two sets, only efficient fluence maps remain in the resulting set  $\hat{X}_E$ . Once the MO-FMO problem has been solved for all BACs  $\mathscr{A} \in \mathcal{A}^*$ , set  $\hat{\mathcal{A}}_E$  is updated so only BACs that have at least one fluence maps  $x \in \hat{X}_E$  will be in  $\hat{\mathcal{A}}_E$  (line 7 in Algorithm 2, where BAC(x) returns the BAC corresponding to the fluence map x). Thus, set  $\hat{\mathcal{A}}_E$  approximates the actual set of efficient BACs of the MO-BAO problem in Equation (8) [2].

## 5. Computational Experiments

We try our three PLS implementations on a prostate case obtained from the CERR package [59] (see Figure 1). We run all our algorithms on an Intel i7 computer with 32 Gb RAM.

Figure 1 shows the three regions considered in this case study: the tumour (prostate), the rectum and the bladder (OARs). The value of the *gEUD* parameter *a* for the tumour, the rectum and the bladder is -10, 8, 2, respectively. These parameters are the same as those used in [2,3,8,16].

In total, more than 20,000 voxels are considered in this prostate case (around 7000 voxels in the tumour, around 5500 in the rectum and around 9500 in the bladder). The number of beamlets (continuous decision variables) ranges between 160 and 220, depending on the considered beam angle. Each BAC consists of N = 5 beam angles (discrete decision variables). We consider a set of 72 equally spaced available coplanar beam angles. The dose deposition matrix A is given. IPOPT [60] is used as our non-linear optimisation solver.

Three sets of initial BACs have been considered. The first set consists of 14 equispaced BACs. The second set of BACs consists of 15 BACs where each beam angle is randomly generated within a predefined range. This is, the first beam angle in an initial BAC,  $\mathscr{A}_1$ , is randomly chosen, so it falls between 0 and 70. The second beam angle,  $\mathscr{A}_2$ , will fall between 75 and 145, and so on. Finally, the third set of initial BACs consists of 15 BACs for which beam angles were chosen completely random (no predefined ranges were considered) [16]. For the second and third sets, where beam angles are randomly selected, we made sure that, on the one hand, no beam angle appears more than once in a BAC and, on the other, all the chosen BACs were multiples of 5 degrees. Table A1 in Appendix A lists these three sets of initial BACs. Since N = 5, the neighbourhood of each BAC consists of 10 BACs which has to be evaluated at each iteration.



Figure 1. Prostate case from CERR. Two OARs (bladder and rectum) are considered.

#### 5.1. Hypevolume Quality Indicator

Since we want to compare the performances of the different implemented algorithms, we need a tool to make this comparison. Unlike in single-objective optimisations where the quality of the algorithm is given by its best solution, in multi-objective optimisation we have a set of (approximately) non-dominated points provided by each algorithm. Then, we need a measure to compare such sets of points.

Over the last two decades, several authors have proposed different quality indicators [61–64] to measure the quality of a set of (approximately) non-dominated points. In this paper, we use the *hypervolume* quality indicator  $\mathscr{S}$  to measure the quality of the set of (approximately) non-dominated points obtained by an algorithm. The hypervolume quality indicator  $\mathscr{S}$  gives the volume of the portion of the objectives space that is weakly dominated by a specific set of (approximately) non-dominated points [63]. It allows the integration of aspects that are individually measured by other metrics. Mathematically, the hypervolume is defined as a function  $\mathscr{S} : \hat{Y}_N \to \mathbb{R}^+_0$ , where  $\hat{Y}_N$  is a set of pairwise non-dominated points in the objective space. The hypervolume is one of the most accepted and used quality indicators in MO optimisation. Thus, we use the hypervolume value as a measure of the performance of each of the implemented algorithms.

Figure 2a shows an example of the entire area dominated by a set of (approximately) non-dominated points (solid circles) in a minimisation problem (both  $f_1$  and  $f_2$  must be minimised). The solid square is our reference point which usually corresponds to some upper bounds of the problem being solved. The hypervolume can be expressed either directly as the value of the dominated area (in this example 1815) or as the % of the imaginary square formed by the ideal point and the reference point. If we consider the ideal point of our example equal to (0, 0), the total area would be 4225, and thus the hypervolume value would be 42.95%. In Figure 2b, we add a second set of non-dominated points and

compare them in terms of their hypervolumes. As we can see, in dark grey is the area that is exclusively dominated by the original set of non-dominated points  $\mathcal{A}$  (solid circles). In the same way, the area that is only dominated by the new set of non-dominated points  $\mathcal{B}$  (solid triangles) is in light grey. Then, we calculate both the total area of  $\mathcal{A}$  and the total area of  $\mathcal{B}$ . The obtained values for this example are 34 and 38, respectively. Then, since we are looking for a set of (approximately) non-dominated points with larger hypervolumes, the set  $\mathcal{B}$  should be preferable to the set  $\mathcal{A}$ . It is interesting to note, though, that set  $\mathcal{A}$  has no point dominated by any point from set  $\mathcal{B}$ . Furthermore, there are two points in  $\mathcal{B}$  that are dominated by at least one point in  $\mathcal{A}$ . Thus, the hypervolume values of two sets  $\mathcal{A}$  and  $\mathcal{B}$  cannot be used to state any dominance relationship among sets and their elements.



**Figure 2.** Examples on how the hypervolume is calculated in a bi-objective space. (**a**) Example of the hypervolume dominated by a set of 6 non-dominated points in the objective space. (**b**) Resulting hypervolume for two sets of non-dominated points.

## 5.2. Results

In this section, we present the results obtained for the experiments performed in this paper. We first show the sample points in the objective space generated by all four algorithms for one initial BAC used in this paper (initial BAC no. 43 in Table A1). Unfilled circles correspond to the sample points belonging to those BACs that were not explored (i.e., no neighbours were generated for these BACs). Solid blue squares are the sample points belonging to explored BACs, i.e., those BACs for which at least one neighbour was generated. Thin blue lines connect a sample point of a BAC to its neighbour BACs sample points. Thicker blue lines connect the sample points of all the explored BACs in the same order they were explored. We call this the *path* of the algorithm. Solid green circles correspond to those non-dominated points that were not explores all the non-dominated points at each iteration. Finally, red triangles correspond to sample points that formed part of the final set of locally non-dominated points. As we can see, sample points for many BACs are generated at each iteration, which means many optimisation problems need to be solved [8].



Figure 3. Sample points generated by PLS algorithm.

As we can see, the PLS algorithm (Figure 3) generates many more sample points than all the other algorithms, which leads to longer run times. For this particular example, the PLS took 57,922 s. (more than 16 h) and need 839 function evaluations. As a result, 10 locally efficient BACs were produced (red triangles in Figure 3).

Figure 4 shows the path for the nPLS algorithm. The nPLS algorithm requires less objective function evaluations than the standard PLS from Figure 3. For this particular example, the nPLS algorithm only performed 456 function evaluations with a run time of 26,405 s. (app. 7 h). As a result, four locally efficient BACs were produced. Remarkably, sample points corresponding to the set of locally efficient BACs found by the nPLS algorithm,  $\mathscr{A}_{nPLS}^*$ , dominate the majority of the points corresponding to the set of locally efficient BACs found by the standard PLS algorithm. Although this situation does not occur for all the experiments performed here, we will see that, on average, the nPLS algorithm performs better than all the other algorithms considered in this paper in terms of its hypervolume value.



Figure 4. Sample points generated by nPLS algorithm.

Figure 5 shows the path followed by the jPLS algorithm presented in this paper. Because the search is driven by the judgement function h value, we can see that the algorithm converges much faster than both the nPLS and the PLS presented before. For this example, the jPLS algorithm only performed 255 function evaluations with a run time of 16,488 s (4.5 h). As a result, six locally efficient BACs were produced. We need to highlight that, although the locally efficient BACs found by the jPLS algorithm are not as good as the ones found by the nPLS algorithm, they are relatively close to the set of locally efficient BACs found by the PLS algorithm in terms of its hypervolume value. The above is important as the jPLS algorithm takes, on average, a third part of the time that the standard PLS algorithm needs to converge to a set of locally efficient BACs. Note that, for one particular iteration, we have a set of BACs that need to be generated. Some of these BACs are not necessarily neighbours of the current solution and neighbours of the current solution are not necessarily the ones with the best judgement function. Unlike the nPLS algorithm, which always chooses the neighbours of the current solution, the jPLS algorithm chooses the BAC in the archive with the best judgement function value. As a consequence, the path both algorithms follow is (usually) very different.

As mentioned before, the rPLS algorithm is considered a baseline algorithm as it does not exploit any problem-specific feature. As we expected, the rPLS algorithm consistently converges to sets of locally efficient BACs that have smaller hypervolume values than all the other MO-LS algorithms (See sample points in Figure 6). Further, the rPLS algorithm is not the fastest algorithm implemented here, as it consistently takes longer than the jPLS algorithm. For the example, the rPLS algorithm took 22,201 s. (more than 6 h) and needed 356 objective function evaluations.



Figure 5. Sample points generated by jPLS algorithm.



Figure 6. Sample points generated by rPLS algorithm.

Finally, we show the path followed by both the single-objective local search algorithms implemented here: steepest descent and next descent (Figures 7 and 8, respectively). As expected, single-objective local search algorithms converge faster (fewer objective function evaluations are needed) at the cost of less locally optimal BACs (only 1 is found for each initial BAC) and smaller hypervolume values. Moreover, although the steepest descent algorithm is, on average, slightly better than the next descent algorithm in terms of both hypervolume and judgement function value, the next descent algorithm is consistently faster than the steepest descent. This makes the next descent algorithm an interesting alternative if one wants to quickly improve the quality of the initial BAC and then perform an MO-LS algorithm such as the standard PLS starting from the locally optimal BAC provided by the next descent algorithm.



Figure 7. Sample points and the path generated by the steepest descent algorithm in objective space.



Figure 8. Sample points and paths generated by the next descent algorithm in objective space.

In Table 2, a summary of the obtained results per each initial BAC is shown. Column # corresponds to the initial BAC identifier according to Table A1. As we mentioned before, 44 initial BACs for each algorithm are considered in our experiments. Column  $\mathscr{S}$  show the hypervolume value of the obtained set of locally efficient solutions. Column  $\hat{X}_E^{\mathscr{A}}$  shows the number of locally efficient solutions obtained starting from the corresponding initial BAC. Column  $\mathcal{N}(\mathscr{A})$  shows the number of explored BACs. Finally, column *fevals* is the number of objective function evaluations the algorithm performs before finding the final set of non-dominated points for each initial BAC—that is, the number of sample points that are calculated by the algorithm.

 $\begin{array}{r}
 14 \\
 14 \\
 6 \\
 5 \\
 10 \\
 5
 \end{array}$ 

		-0	PL Î d	S	(	-0	rPl	S	(	-0	jPI	LS	(T. 1	-0	nPl	LS	(
	#	S	$X_E^{sa}$	Л	f Eval	9	$X_E^{sa}$	Л	f Eval	9	$X_E^{\omega}$	Л	f Eval	9	$X_E^{\omega}$	Л	f Eval
Equally distant BACs	$     \begin{array}{r}       1 \\       2 \\       3 \\       4 \\       5 \\       6 \\       7 \\       8 \\       9 \\       10 \\       11 \\       12 \\       13 \\       14 \\     \end{array} $	83.560 83.560 83.076 83.076 83.076 83.076 83.076 83.076 83.076 83.560 83.560 83.560 83.560 83.560	$     \begin{array}{r}       4 \\       4 \\       4 \\       8 \\       9 \\       9 \\       9 \\       9 \\       9 \\       9 \\       9 \\       4 \\     $	33 55 82 35 27 54 63 58 57 75 46 43 40 28	250 379 576 260 207 358 400 383 393 529 333 297 272 208	$\begin{array}{c} 83.560\\ 83.560\\ 83.076\\ 83.076\\ 83.076\\ 83.076\\ 83.076\\ 83.076\\ 83.076\\ 83.560\\ 83.560\\ 83.560\\ 83.560\\ 83.560\\ 83.560\\ 83.560\end{array}$	$\begin{array}{c} 4 \\ 4 \\ 4 \\ 8 \\ 8 \\ 8 \\ 8 \\ 8 \\ 8 \\ 8 \\$	24 27 27 21 20 18 20 27 24 31 22 19 13 14	197 221 223 171 159 147 161 206 191 251 182 155 110 115	$\begin{array}{c} 83.560\\ 83.560\\ 83.056\\ 83.056\\ 83.056\\ 83.056\\ 83.056\\ 83.056\\ 83.056\\ 83.056\\ 83.056\\ 83.560\\ 83.560\\ 83.560\\ 83.560\\ 83.560\\ \end{array}$	$\begin{array}{c} 4 \\ 4 \\ 4 \\ 8 \\ 8 \\ 8 \\ 8 \\ 8 \\ 8 \\ 8 \\$	26 25 29 22 21 18 21 22 23 39 17 15 14 13	206 202 246 178 171 148 170 178 187 313 144 125 118 112	$\begin{array}{c} 83.560\\ 83.560\\ 83.074\\ 83.074\\ 83.074\\ 83.074\\ 83.076\\ 83.074\\ 83.074\\ 83.560\\ 83.560\\ 83.560\\ 83.560\\ 83.560\\ 83.560\\ \end{array}$	$\begin{array}{c} 4 \\ 4 \\ 4 \\ 8 \\ 8 \\ 8 \\ 9 \\ 8 \\ 8 \\ 9 \\ 8 \\ 8 \\ 4 \\ 4 \\ 4 \\ 4 \\ 4 \\ 4 \\ 4 \\ 4$	20 21 37 22 20 16 20 21 23 24 19 15 14 13	$\begin{array}{c} 168 \\ 177 \\ 299 \\ 178 \\ 164 \\ 130 \\ 156 \\ 167 \\ 183 \\ 200 \\ 157 \\ 126 \\ 117 \\ 110 \end{array}$
Semi-Random BACs	15 16 17 18 19 20 21 22 23 24 25 26 27 28 29	83.076 83.560 83.560 83.681 83.392 83.076 83.328 83.681 83.681 83.681 83.681 83.681 83.681 83.681 83.681 83.076	9 4 4 4 8 10 9 6 8 4 8 8 6 8 9	$\begin{array}{c} 68\\ 112\\ 72\\ 198\\ 50\\ 67\\ 103\\ 21\\ 102\\ 77\\ 55\\ 69\\ 145\\ 97\\ 52\\ \end{array}$	$\begin{array}{r} 476\\794\\461\\1257\\338\\505\\710\\170\\694\\509\\336\\459\\1051\\646\\355\end{array}$	83.076 83.560 83.560 82.722 83.681 82.849 82.385 83.377 83.560 82.849 82.849 83.560 82.849 83.560 82.849 83.076	8 4 4 10 8 4 9 6 8 4 8 8 4 8 8 8 8 8	34 32 30 55 23 16 33 19 74 28 21 38 33 42 22	269 268 234 428 185 130 256 157 566 237 167 284 271 336 175	83.076 83.560 82.575 83.681 82.849 82.490 83.377 83.067 83.560 83.681 83.681 83.560 83.681 83.681 83.681 83.076	$     \begin{array}{r}       8 \\       4 \\       4 \\       4 \\       8 \\       6 \\       4 \\       6 \\       5 \\       4 \\       8 \\     $	29 39 23 41 21 19 26 19 41 26 18 29 25 38 23	240 326 190 343 175 157 219 162 339 217 150 239 214 313 189	83.076 83.560 83.560 83.681 83.377 83.076 83.076 83.377 82.777 83.681 83.681 83.560 83.501 83.076	9 4 4 4 8 6 8 6 4 6 8 6 4 6 8 8 4 4 8 8 4 4 8	43 38 23 30 28 30 17 35 46 24 30 31 32 21	335 320 190 262 240 232 247 142 288 371 190 242 254 265 170
Completely Random BACs	30 31 32 33 34 35 36 37 38 39 40 41 42 43	81.758 83.940 83.377 83.560 83.076 83.667 83.914 83.685 83.918 83.278 83.278 83.278 83.224 81.758 83.918 83.914	$ \begin{array}{c} 6\\ 7\\ 6\\ 4\\ 8\\ 12\\ 10\\ 9\\ 5\\ 14\\ 14\\ 6\\ 5\\ 10\\ \end{array} $	67 30 138 95 92 89 35 54 65 43 92 55 81 122	473 206 936 642 639 591 253 351 445 318 613 425 543 839	$\begin{array}{c} 81.758\\ 83.940\\ 83.377\\ 83.560\\ 83.076\\ 82.050\\ 83.914\\ 83.076\\ 83.805\\ 83.278\\ 81.785\\ 81.785\\ 81.758\\ 83.805\\ 82.849\\ \end{array}$	$ \begin{array}{c} 6\\ 7\\ 6\\ 4\\ 8\\ 12\\ 10\\ 9\\ 5\\ 14\\ 14\\ 6\\ 5\\ 4\\ \end{array} $	$\begin{array}{c} 37\\18\\43\\41\\32\\37\\21\\18\\32\\30\\38\\46\\29\\45\end{array}$	301 146 352 331 262 291 164 143 258 232 296 366 240 356	$\begin{array}{c} 81.758\\ 83.940\\ 83.377\\ 83.560\\ 83.076\\ 82.050\\ 83.914\\ 83.076\\ 83.805\\ 83.688\\ 81.785\\ 81.785\\ 81.758\\ 83.805\\ 83.337\end{array}$	$ \begin{array}{r} 6\\ 7\\ 6\\ 4\\ 8\\ 12\\ 10\\ 8\\ 5\\ 4\\ 14\\ 6\\ 5\\ 6\\ \end{array} $	32 17 44 36 32 35 20 17 31 43 30 32 25 30	265 138 361 289 266 289 164 138 252 355 243 269 213 255	$\begin{array}{c} 81.758\\ 83.940\\ 83.377\\ 83.560\\ 83.076\\ 82.050\\ 83.914\\ 83.076\\ 83.805\\ 83.278\\ 81.785\\ 81.785\\ 81.758\\ 83.805\\ 83.972\\ \end{array}$	$ \begin{array}{c} 6 \\ 7 \\ 6 \\ 4 \\ 8 \\ 12 \\ 10 \\ 8 \\ 5 \\ 14 \\ 14 \\ 6 \\ 5 \\ 4 \\ \end{array} $	29 18 39 37 30 31 22 18 33 30 39 40 26 56	$\begin{array}{c} 237\\ 144\\ 325\\ 299\\ 249\\ 252\\ 173\\ 146\\ 265\\ 222\\ 304\\ 327\\ 221\\ 456\\ \end{array}$

Table 2. Results for MO-LS algorithms for all instances.

From Table 2, we have that, on average, the PLS algorithm obtains the best hypervolume value (83.348%), followed by the nPLS algorithm with 83.259%, the jPLS algorithm with 83.208% and the rPLS algorithm with 83.158%. Moreover, the PLS algorithm is the one that more function evaluations perform with an average of 490, which corresponds to 71 BACs being explored. The nPLS algorithm performs, on average, 228 function evaluations which correspond to 28 BACs being explored. The jPLS algorithm is the fastest algorithm, with 224 function evaluations on average and 27 explored BACs. Finally, the rPLS performs 240 function evaluations and explores 30 BACs on average, being the slower algorithm among the PLS-based algorithms proposed in this paper. Although the number of function evaluations varies from one algorithm to the other, the number of locally efficient BACs that each algorithm found for each initial BAC is, on average, very similar: The PLS algorithm found 7 locally efficient BACs per initial BAC. The same occurs for the nPLS and the rPLS algorithms, while for the jPLS, 6 locally efficient BACs were found on average for each initial BAC.

82.455

Analysing Table 2, we have that, for the set of equispaced BACs, all four algorithms converge to the same set of locally efficient BACs for several initial BACs. In addition, we can note that different initial BACs converge to the same set of locally optimal BACs.

Figure 9 shows the path followed by the jPLS algorithm in the objective space for several initial BACs from the set of equispaced BACs. Unlike in Figures 3–6, where the generated sample points are shown, Figure 9 only shows the sample points of those BACs for which its neighbourhood was explored. Here, we can see how when the jPLS algorithm starts from initial BACs 0, 1, 2, 10, 11, 12, 13 from Table 2, it converges to the same set of locally efficient BACs. This is because of the similarity of this set of initial BACs in terms of their beam angles values. Although the jPLS algorithm follows different paths in the

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82.455

objective space for each initial BAC, i.e., it explores different BACs and always converges to the same set of locally efficient BACs. A similar situation occurs for the remaining equispaced initial BACs (numbered from 3 to 9), where the jPLS algorithm also converges to the same set of locally efficient BACs. This set is different from the one showed in Figure 9, though. This situation also occurs for the other algorithms, which converge to similar sets of locally efficient BACs. As long as more variety is included in the initial BACs, the situation described in Figure 9 tends to disappear. For instance, for the 15 initial BACs in the set of completely random initial BACs (numbered from 30 to 44 in Table 2), we obtain 14 different sets of locally efficient BACs. There are only two initial BACs (34 and 37 in Table 2) that converge to the same set. When we look at these two initial BACs, we can see that they are very similar in that they have the same beam angle  $\mathscr{A}_1 = 20^\circ$  and the difference in the other beam angles is relatively small ( $20^{\circ}$  for  $\mathscr{A}_2$ ,  $20^{\circ}$  for  $\mathscr{A}_2$ ,  $30^{\circ}$  for  $\mathscr{A}_3$ ,  $25^{\circ}$  for  $\mathscr{A}_4$  and  $15^{\circ}$  for  $\mathscr{A}_5$ ). Thus, because we want to produce as many locally efficient BACs as possible to provide more alternatives for the decision maker to choose from, we should avoid initial BACs that are too similar in terms of the beam angles that are part of it, as they are likely to converge to the same or too similar locally efficient BACs.



**Figure 9.** jPLS paths in objective space for the initial BACs 0-2 and 10-13 in Table A1. All the initial BACs end up in the same set  $\mathscr{A}^*$  of locally efficient BACs.

Figure 10a,c,e show the hypervolumes obtained for all algorithms for the equispaced, semi-random and completely random initial BACs, respectively. Although both the steepest descent and next descent algorithms can obtain better hypervolume values than the MO-LS algorithms for some few initial BACs, this is not the general case. In fact, for most experiments, results obtained by the single-objective local search algorithms are even below the ones obtained by the rPLS algorithm. We expected this as a single-objective local search algorithm performs fewer function evaluations and, thus, does not explore the search space as MO-LS algorithms do.



**Figure 10.** Hypervolume per algorithm. (**a**) Hypervolume for all algorithms for equispaced initial BACs (0–13). (**b**) Cumulative hypervolume for all algorithms for equispaced initial BACs (0–13). (**c**) Hypervolume for all algorithms for semi-random initial BACs (14–29). (**d**) Cumulative hypervolume for all algorithms for semi-random initial BACs (14–29). (**e**) Hypervolume for all algorithms for random initial BACs (30–44). (**f**) Cumulative hypervolume for all algorithms for random initial BACs (30–44).

Moreover, we calculate the *cumulative hypervolume*, i.e., the hypervolume that is obtained after merging the obtained set of locally efficient BACs of each initial BAC. We do this for each algorithm and keep the same order as in Table 2. We calculate an independent cumulative hypervolume for each set of initial BACs (the equispaced, semi-random and completely random initial BACs). Figure 10b,d,f show the cumulative hypervolume value for each algorithm. Unlike in Figure 10a,c,e, where the *x* axis identifies the number of the initial BACs, the *x* axis in Figure 10b,d,f corresponds to the cumulative number of objective function evaluations that are needed to obtain the corresponding cumulative hypervolume

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value. As we can see, single-objective local search algorithms increase their cumulative hypervolume value rapidly. However, their final cumulative hypervolume value is always far below the values obtained by the MO-LS algorithms. Although the order in which the initial BACs are considered might affect how the cumulative hypervolume increases, it is clear that MO-LS obtains better hypervolume values than single-objective local search algorithms. It is interesting to note that for the completely random set of initial BACs, the PLS algorithm not only is the one that takes longer to obtain its final set of locally efficient solutions but also it does not obtain the best cumulative hypervolume value, as the nPLS algorithm obtains a slightly better value almost half of the time.

# 6. Conclusions and Future Work

In this paper, the MO-BAO problem is solved using three MO-LS algorithms derived from the well-known Pareto Local Search algorithm. These MO-LS algorithms are used within the two-phase framework we proposed in [2]. We demonstrate that when replacing the single-objective local search in phase one of the two-phase approach by MO-LS algorithms, the obtained set of locally efficient BACs improves in terms of the obtained hypervolume value, although MO-LS algorithms require more function evaluations. Moreover, exploiting problem features such as the judgement function value of BACs (jPLS algorithm) or the neighbouring relationships among BACs (nPLS algorithm) is very effective in finding promising BACs. However, one drawback of using MO-LS algorithms during the first phase of the two-phase approach is that many objective function evaluations are needed. This is especially true for the standard Pareto local search implemented here. As expected, the three variations proposed in this paper are much faster than the PLS algorithm, as they require fewer function evaluations. However, the time they need to converge is still prohibitive in clinical practice. To overcome this issue, as future work, we propose combining single- and multi-objective local searches such that a single-objective local search can provide good starting points to the MO-LS algorithms. Moreover, perturbing a local search to avoid being trapped in locally optimal sets is also an exciting research line to be explored in future work too.

Author Contributions: Conceptualisation, G.C.-G.; methodology, G.C.-G. and C.L.; software, G.C.-G. and C.L.; validation, C.L.; data curation, G.C.-G. and C.L.; writing, G.C.-G. and C.L.; supervision, G.C.-G. All authors have read and agreed to the published version of the manuscript.

Funding: This research was funded by the FONDECYT grant number 1211129.

**Institutional Review Board Statement:** Ethical review and approval were waived for this study, as it is a retrospective study on fully anonymised data.

Informed Consent Statement: Not applicable.

Data Availability Statement: Not applicable.

Conflicts of Interest: The authors declare no conflict of interest.

## Appendix A

In this appendix, Table A1 shows the three sets of instances considered in this paper.

		$\mathcal{A}_1$	$\mathcal{A}_2$	$\mathcal{A}_3$	$\mathscr{A}_4$	$\mathcal{A}_5$
	1	0	70	140	210	280
	2	5	75	145	215	285
	3	10	80	150	220	290
$\mathbf{C}$	4	15	85	155	225	295
BA	5	20	90	160	230	300
nt ]	6	25	95	165	235	305
sta	7	30	100	170	240	310
ib	8	35	105	175	245	315
lly	9	40	110	180	250	320
lua	10	45	115	185	255	325
E	11	50	120	190	260	330
	12	55	125	195	265	335
	13	60	130	200	270	340
	14	65	135	205	275	345
	15	55	95	205	250	305
	16	50	135	175	240	335
	17	60	80	200	255	335
s	18	40	115	190	230	355
JO I	19	35	135	165	250	305
$\mathbf{B}_{I}$	20	70	120	150	240	350
шс	21	70	100	155	290	310
ndı	22	60	100	150	220	335
Rai	23	20	140	190	240	305
ni-	24	60	80	185	250	330
Ser	25	25	125	155	255	300
•	26	35	130	175	275	300
	27	60	115	175	245	345
	28	35	145	170	280	320
	29	35	105	165	235	320
	30	5	40	230	275	340
	31	95	210	245	270	340
ŝ	32	30	120	130	170	345
AC	33	80	155	265	270	335
υB	34	20	125	185	220	305
lon	35	10	45	125	155	305
anc	36	80	140	205	245	330
R	37	20	105	155	245	290
ely	38	155	210	275	315	325
let	39	135	175	210	275	355
du	40	80	115	130	320	345
<u></u>	41		30	225	245	33U 210
<u> </u>	42	215	230	245	285	310
	43	55	105	185	225 21 5	33U 275
	44	U	15	40	215	2/5

Table A1. Sets of instances used in this paper.

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