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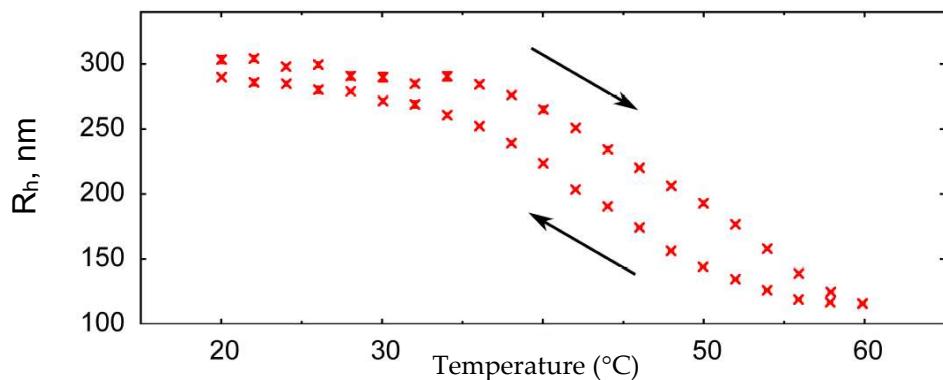
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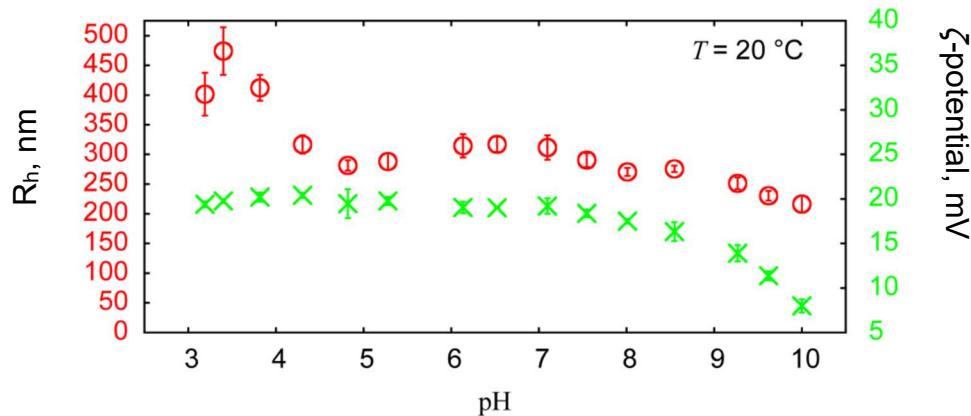
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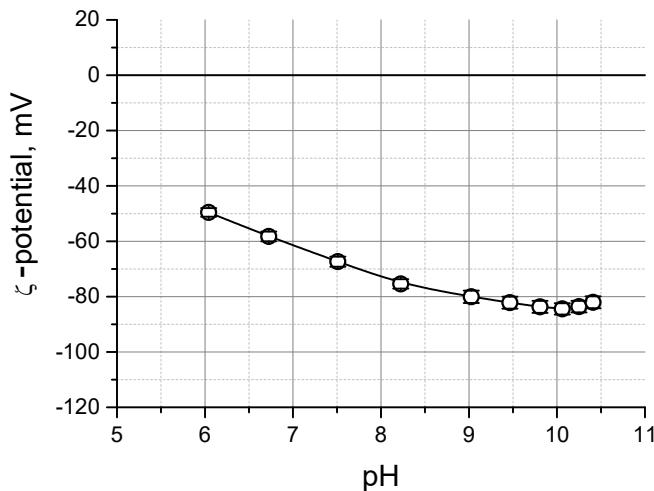
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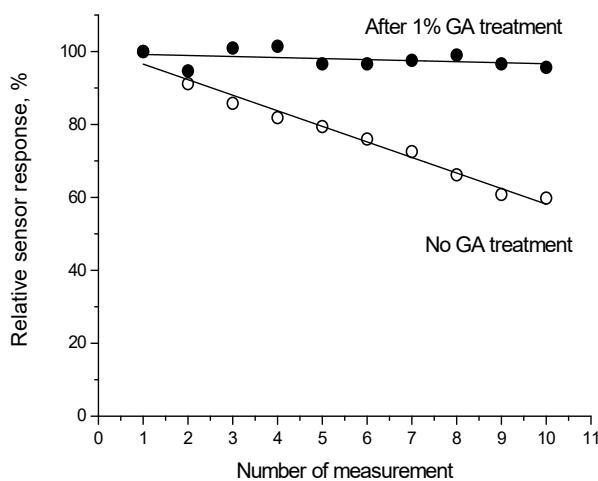
**Figure S1.** The temperature dependence of the hydrodynamic radius of poly(*N*-isopropylacrylamide-*co*-*N*-[3-(dimethylamino)propyl]methacrylamide) (P[NIPAM-*co*-DMAPMA]) microgel particles.



**Figure S2.** The pH-dependences of the hydrodynamic radius and  $\zeta$ -potential of P(NIPAM-*co*-DMAPMA) microgel particles.



**Figure S3.** The pH-dependence of the surface  $\zeta$ -potential of the poly(vinyl chloride) (PVC) film as measured by electrokinetic analysis (EKA).



**Figure S4.** The relative biosensor responses of the screen-printed electrodes (SPE)/MnO<sub>2</sub>/P(NIPAM-*co*-APMA)/ChO construct (open circles) and the SPE/MnO<sub>2</sub>/P(NIPAM-*co*-APMA)/ChO construct cross-linked with glutaraldehyde (GA) (solid circles) to consecutive additions of choline solution, with the concentration of  $5 \times 10^{-5}$  M. The operational stability was characterized quantitatively as a percentage of change of the biosensor response per a single measurement, and was calculated according to the formula:  $\Delta I = 100\% \times \text{tg}I/I_1$ , where  $\text{tg}I$  is the slope of the dependence of the biosensor response on the number of measurements, normalized to the initial biosensor response  $I_1$  and given in percent.