

Abstract

# Towards Next-Generation Glucose Sensors: Reactively Sputtered Nanostructured Nickel Nitrides for CMOS Integration <sup>†</sup>

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**Abstract:** A facile and clean-room compatible approach to Ni nitride ( $\text{Ni}_x\text{N}_y$ ) synthesis is proposed, based on a reactive sputtering deposition technique.  $\text{Ni}_x\text{N}_y$  thin films were deposited at different  $\text{N}_2$  partial pressures, after which their electrocatalytic properties towards glucose oxidation were investigated. Relative to the bare Ni,  $\text{Ni}_x\text{N}_y$  thin films sputtered at low  $\text{N}_2$  partial pressures exhibited a decreased linear range (0–5 mM) and sensitivity. Contrarily,  $\text{Ni}_x\text{N}_y$  thin films sputtered at high  $\text{N}_2$  partial pressures displayed an increase in sensitivity of  $\approx 30\%$  in the same linear range (0–10 mM) as for Ni. The  $\text{Ni}_x\text{N}_y$  films showed a clear morphological change from a flat thin film (Ni) to a faceted nanostructure whose characteristic dimensions decreased with increasing  $\text{N}_2$ .

**Keywords:** glucose; non-enzymatic sensing; nickel nitride

## 1. Introduction

Detecting glucose levels accurately and sensitively in biofluids is vital for the proper clinical management of diabetes, personal health, and fitness [1]. Despite remarkable efforts towards the development of minimally invasive, miniaturized and reliable sensors for glucose monitoring, most devices continue to rely on an enzyme to mediate the electrooxidation of glucose [1]. Limited by poorly stable as well as pH- and oxygen-sensitive enzymes, this particular field is in dire need of novel non-enzymatic solutions [1]. Recently, transition metal nitrides have attracted increasing interest as catalysts for glucose electrooxidation. Of these, nickel nitrides are particularly intriguing due to their resistance to chloride poisoning [2], biocompatibility, electrical conductivity, thermal and chemical stability [2]. The most common methods of synthesis are via ammonolysis in a  $\text{NH}_3$  atmosphere at high temperatures ( $>300^\circ\text{C}$  for crystal phases) or via a solvothermal method involving toxic species [3]. In contrast, an RF magnetron sputtering system does not require any harmful chemicals and can be performed at room temperature [3], thus being more compatible for the fabrication of integrated sensors. Moreover, by adjusting the sputtering parameters of thin films with different crystal phases and significantly different catalytic activities can be obtained. Although promising, this method is yet to be applied in the development of non-enzymatic glucose sensors in view of an easy integration with electronics.

## 2. Materials and Methods

All electrochemical measurements were taken by means of an *Autolab* potentiostat (PGSTAT204, Metrohm, Kontich, Belgium) in a 3-electrode configuration. The reference electrode was a standard  $\text{Ag}/\text{AgCl}/\text{KCl}_{\text{sat}}$  electrode (Sigma Aldrich, St. Louis, MO, USA), the counter electrode was a Pt coil (Sigma Aldrich). The working electrode was a  $7\text{ mm} \times 7\text{ mm}$   $\text{Ni}_x\text{N}_y$  on borosilicate glass electrode connected a tantalum clip (Redoxme).



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### 3. Discussion

The electrical resistivity of the Ni film was  $100 \mu\Omega\cdot\text{cm}^{-1}$ , in accordance with other works [4]. Both  $\text{Ni}_x\text{N}_y$  thin films displayed similar resistivities of roughly  $300 \mu\Omega\cdot\text{cm}^{-1}$ . Our electrochemical study showed that the electrical measurements were not a predictor for the glucose electrocatalytic activity.

**Morphological characterization:** Unlike for the  $\text{Ni}_x\text{N}_y$  thin films, the pure Ni samples grew with a Volmer Weber growth, leading to partially connected grains. Cubic-like structures fully covered the surface of the  $\text{Ni}_x\text{N}_y$  (20%) and  $\text{Ni}_x\text{N}_y$  (50%) samples, with particularly smaller nanostructures present in the latter (Figure 1).

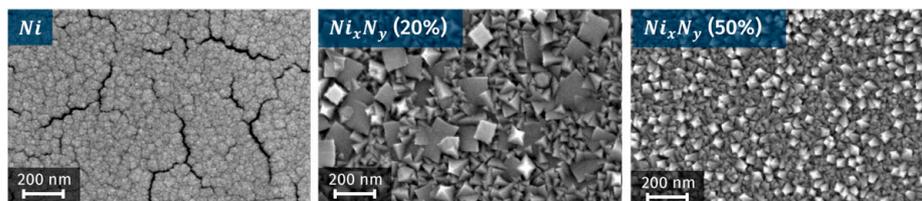


Figure 1. (From left to right) SEM images of Ni,  $\text{Ni}_x\text{N}_y$  (20%),  $\text{Ni}_x\text{N}_y$  (50%).

**Electrochemical characterization:** For all samples, we extended the potential window to more cathodic and anodic potentials and observed no significant effect on the glucose oxidation current. Thus, we kept the potential window at  $[-0.2 \text{ V to } 0.8 \text{ V}]$ . Although the bare Ni was the least resistive, the  $\text{Ni}_x\text{N}_y$  (50%) sample exhibited a 30% lower Ni(II)/Ni(III) peak separation  $\Delta V$  relatively to bare Ni and a 30% overall increase in sensitivity towards glucose. The  $\text{Ni}_x\text{N}_y$  (20%) sample showed a linear range limited to 5 mM (instead of 10 mM) and more than double the  $\Delta V$  (Figure 2).

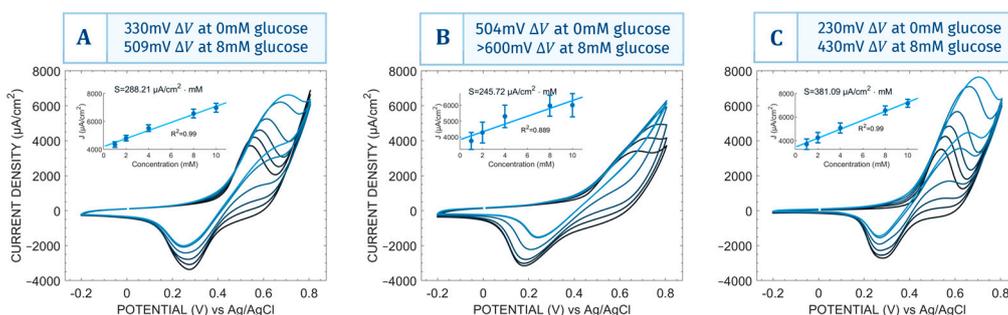


Figure 2. Cyclic voltammograms of Ni (A)  $\text{Ni}_x\text{N}_y$  20% (B),  $\text{Ni}_x\text{N}_y$  50% (C) in 0.1 M KOH at 0, 1, 2, 4, 8, 10 mM of glucose.

### 4. Conclusions

This work depicts the first steps in the development of reactively sputtered  $\text{Ni}_x\text{N}_y$  thin films for non-enzymatic glucose sensing. We observed that a 50% partial pressure of  $\text{N}_2$  during sputtering significantly increases the electrocatalytic activity. Our results set the groundwork for the fabrication of fully integrated glucose sensors without the need for high temperatures or toxic chemicals.

**Author Contributions:** Conceptualization, F.F., C.F. and I.T.; methodology, F.F., C.F. and I.T.; software, F.F.; validation, F.F., C.F. and I.T.; formal analysis, F.F., C.F. and I.T.; investigation, F.F., C.F. and I.T.; resources, F.F.; data curation, F.F.; writing—original draft preparation, F.F.; writing—review and editing, F.F. and C.F.; visualization, F.F.; supervision, I.T. All authors have read and agreed to the published version of the manuscript.

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